

Compressive Sensing

Gabriel Peyré



www.numerical-tours.com



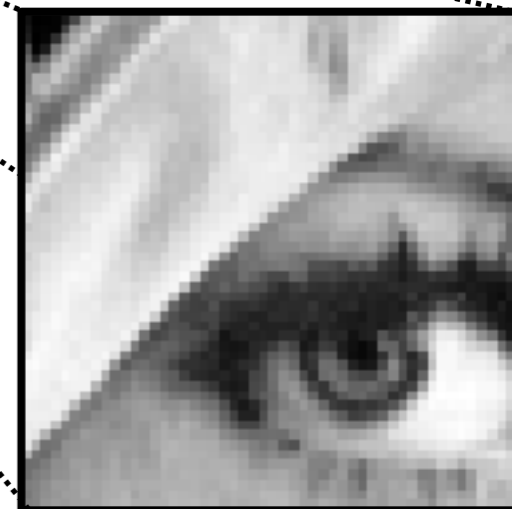
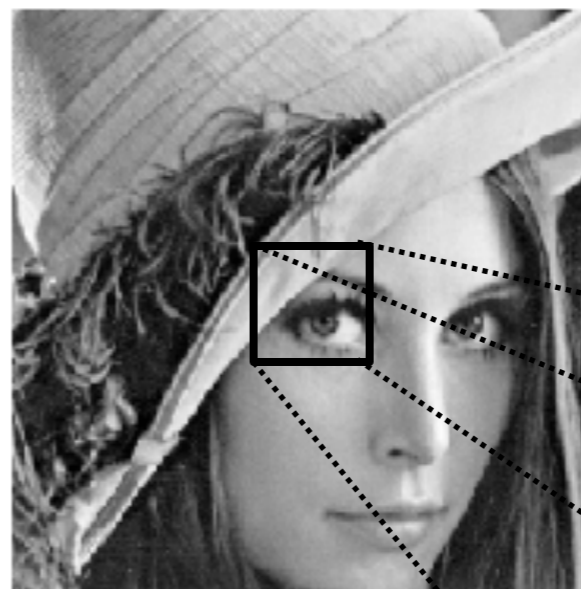
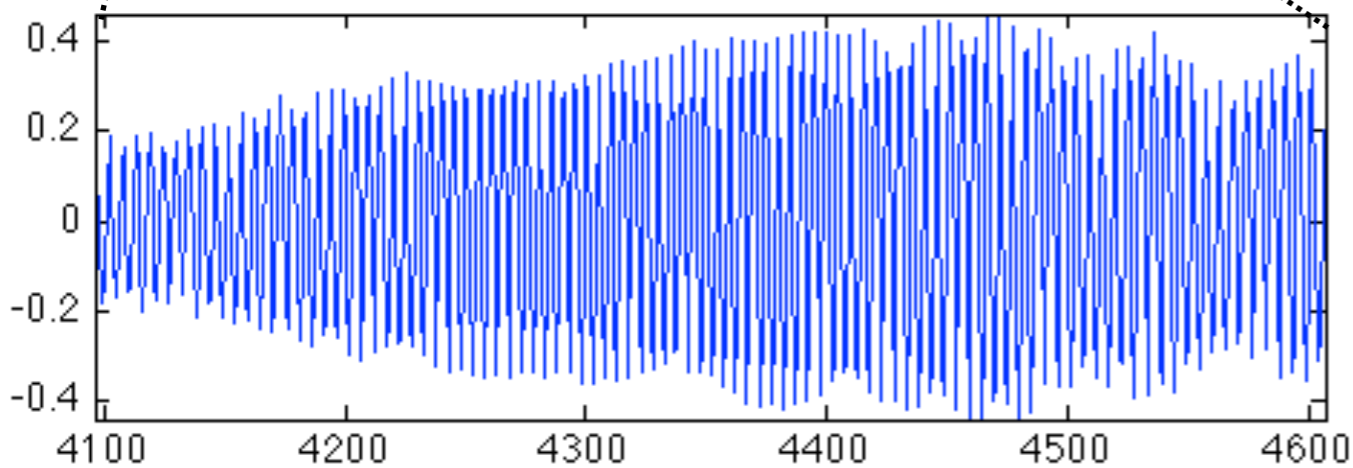
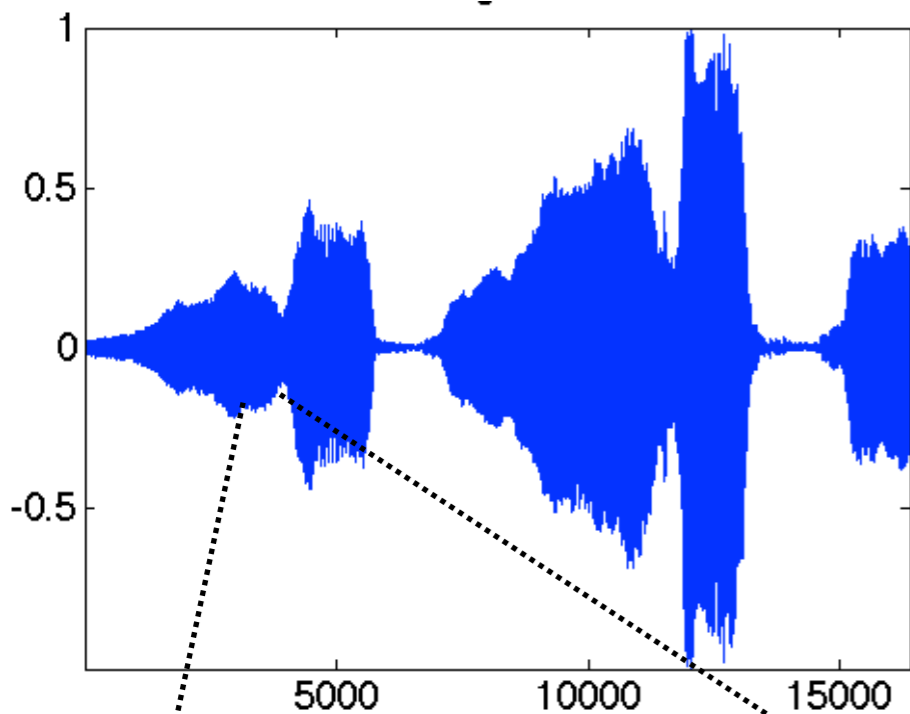
- **Shannon's World**
- Compressive Sensing Acquisition
- Compressive Sensing Recovery
- Theoretical Guarantees
- Fourier Domain Measurements

Discretization

Sampling:

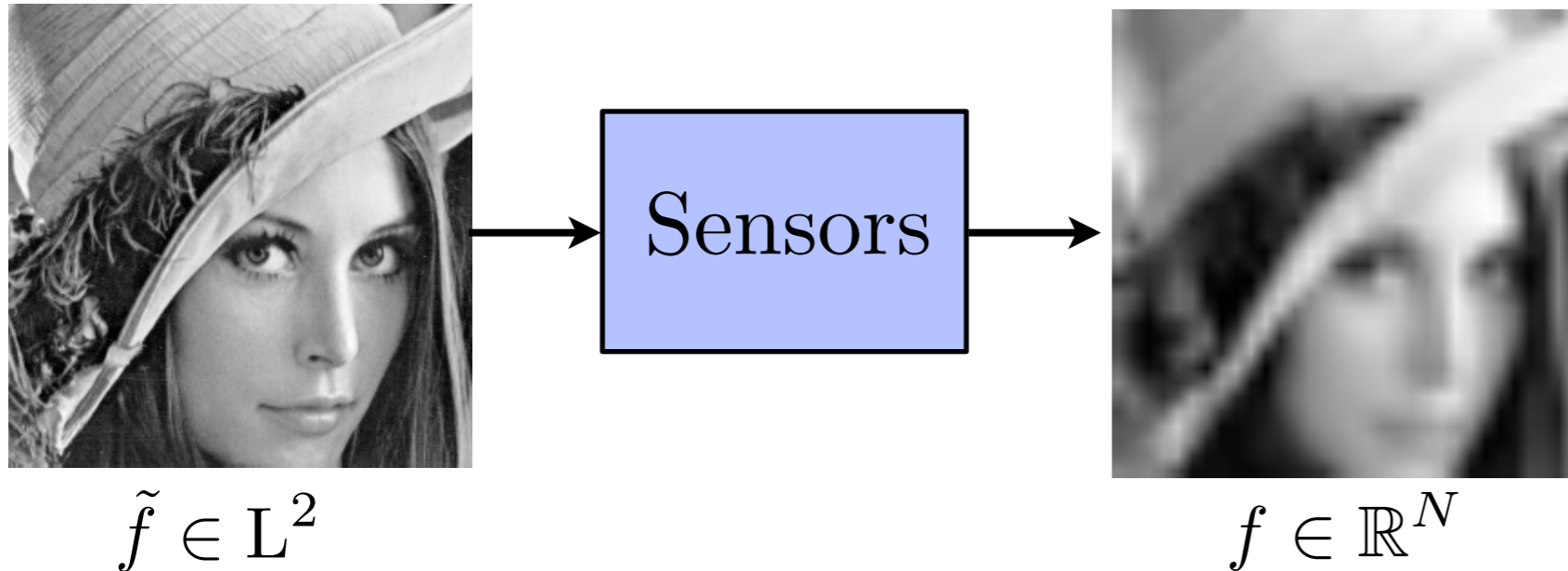
$$\tilde{f} \in L^2([0, 1]^d) \xrightarrow[\text{device}]{\text{acquisition}} f \in \mathbb{R}^N$$

Idealization: $f[n] \approx \tilde{f}(n/N)$



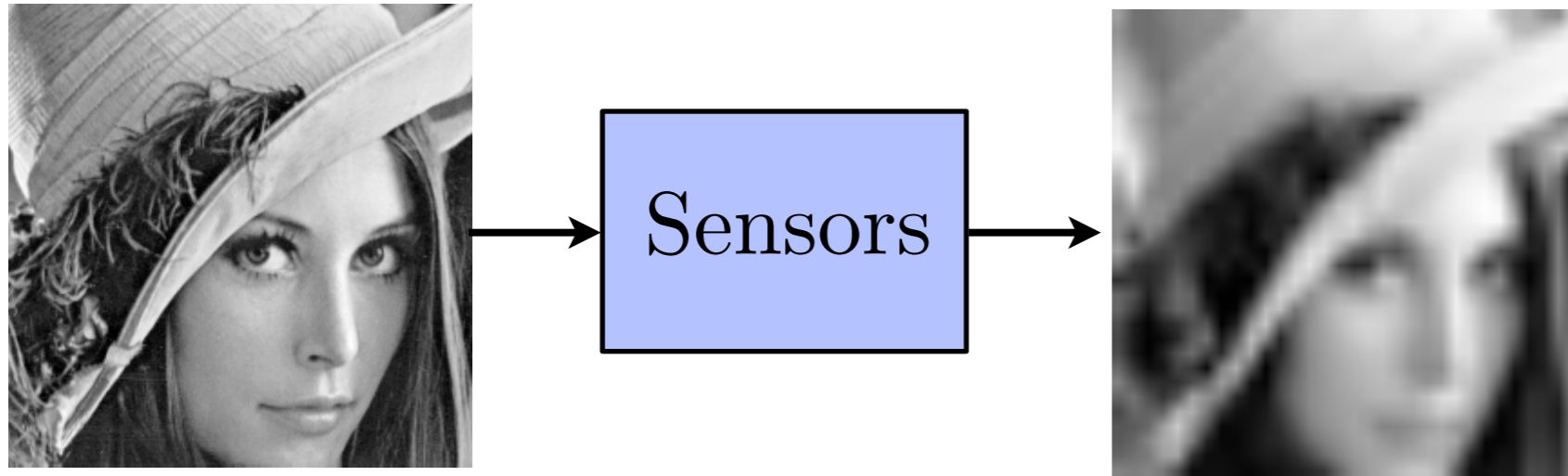
Pointwise Sampling and Smoothness

Data acquisition: $f[i] = \tilde{f}(i/N)$



Pointwise Sampling and Smoothness

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$$\tilde{f} \in L^2$$

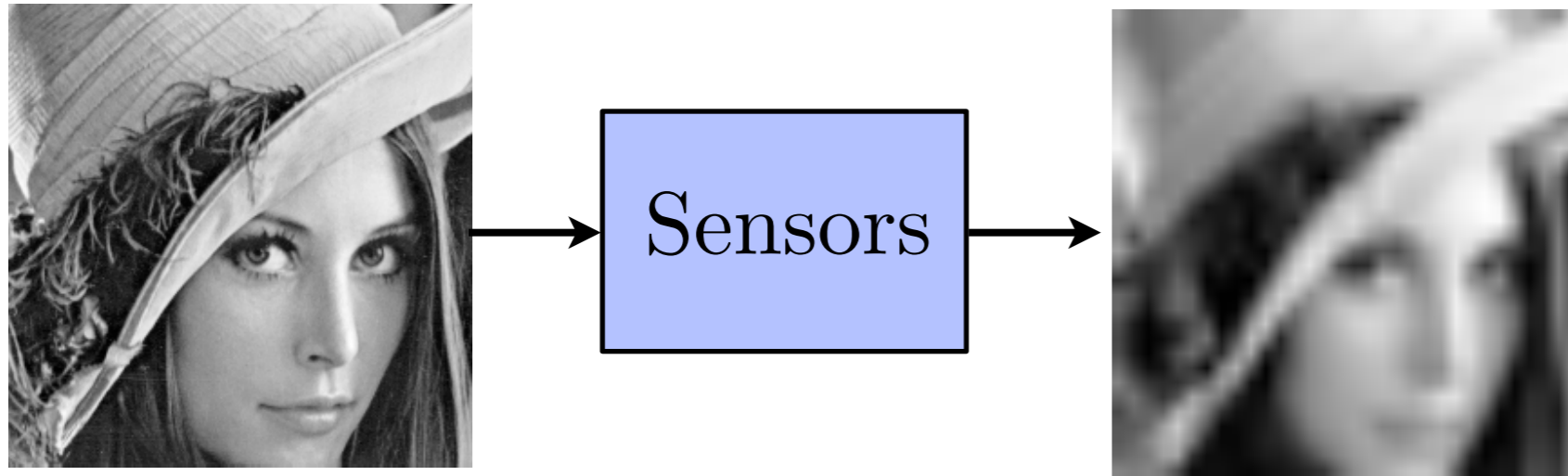
$$f \in \mathbb{R}^N$$

Shannon interpolation: if $\text{Supp}(\hat{\tilde{f}}) \subset [-N\pi, N\pi]$

$$\tilde{f}(t) = \sum_i f[i] h(Nt - i) \quad h(t) = \frac{\sin(\pi t)}{\pi t}$$

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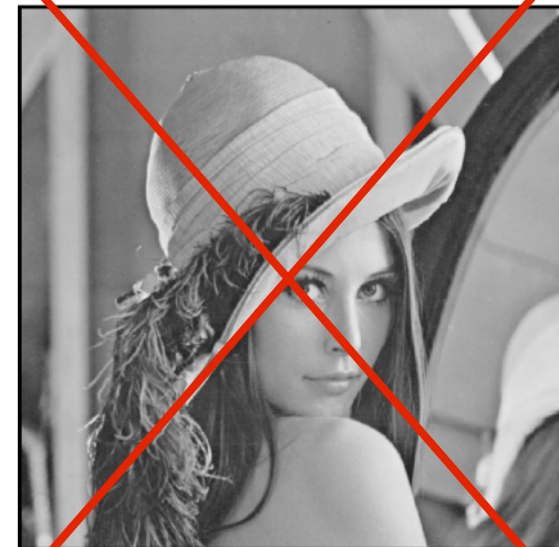
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→ Natural images are not smooth.



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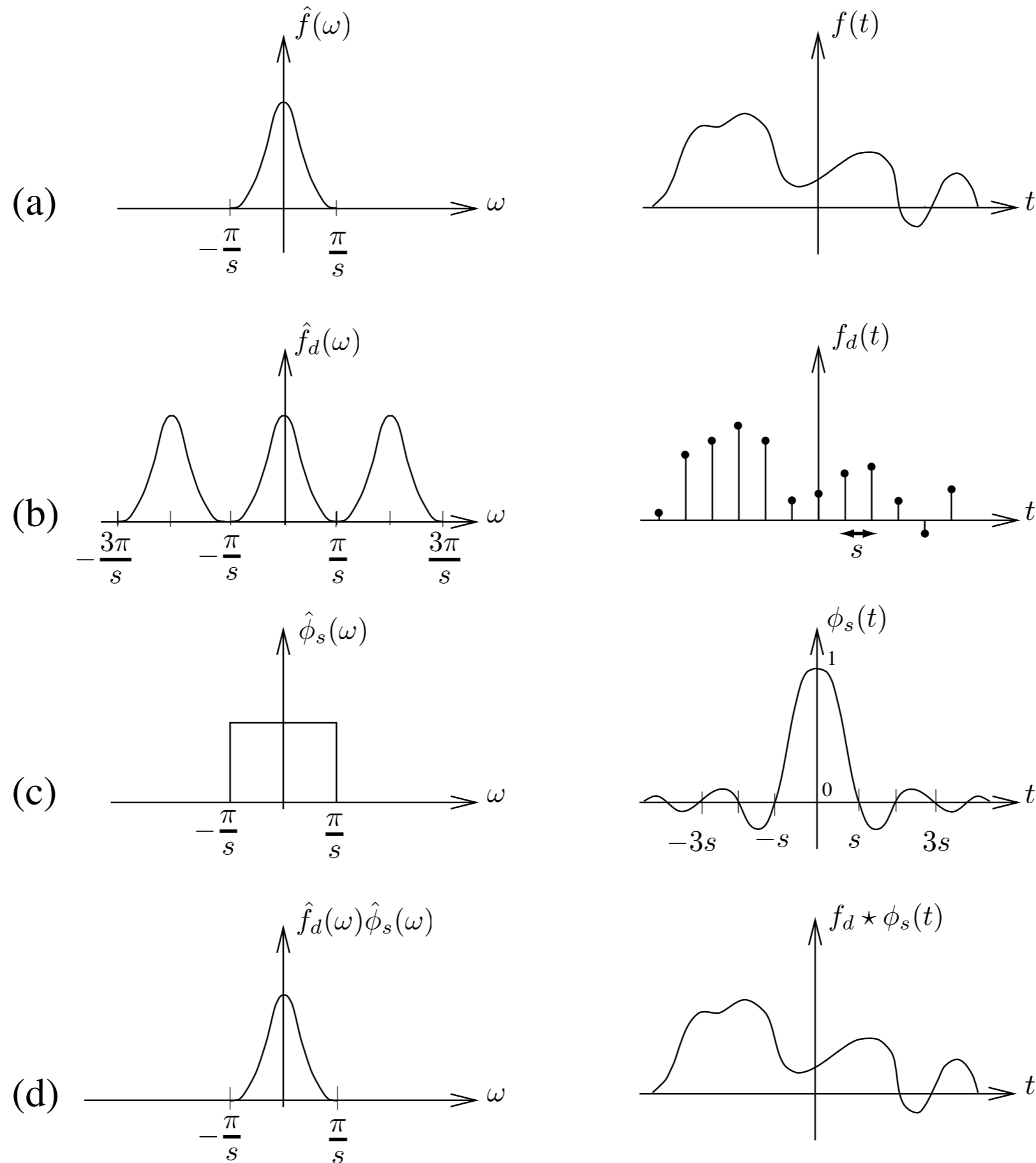
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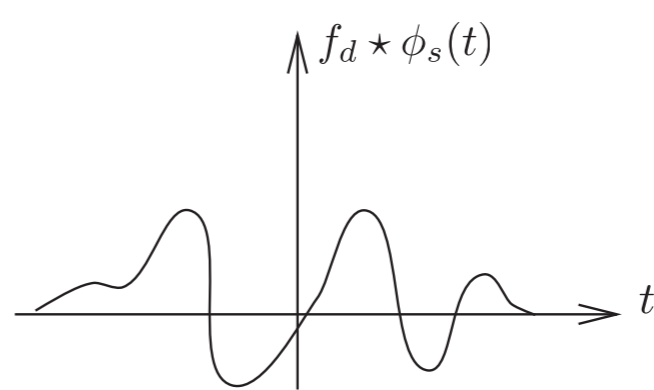
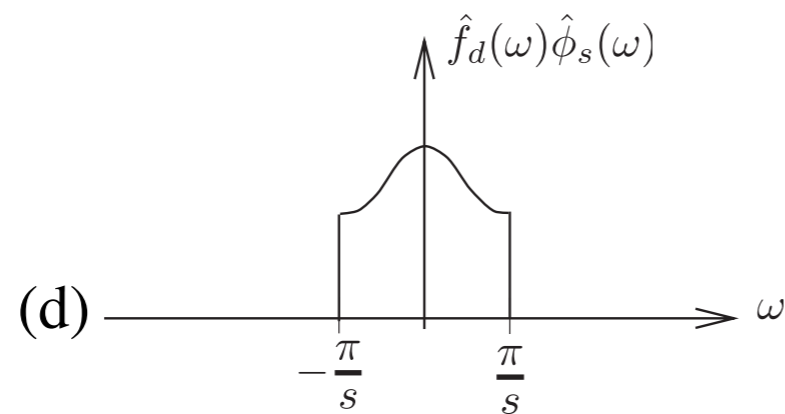
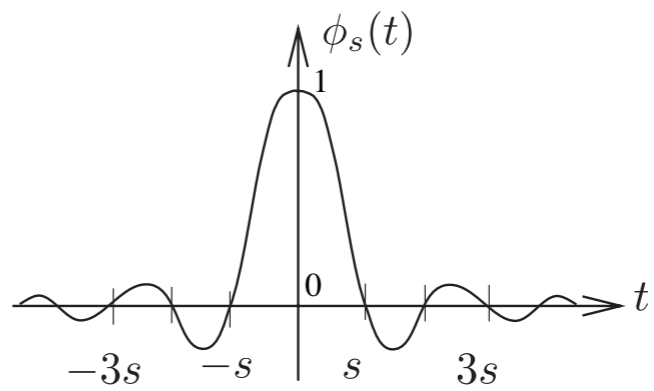
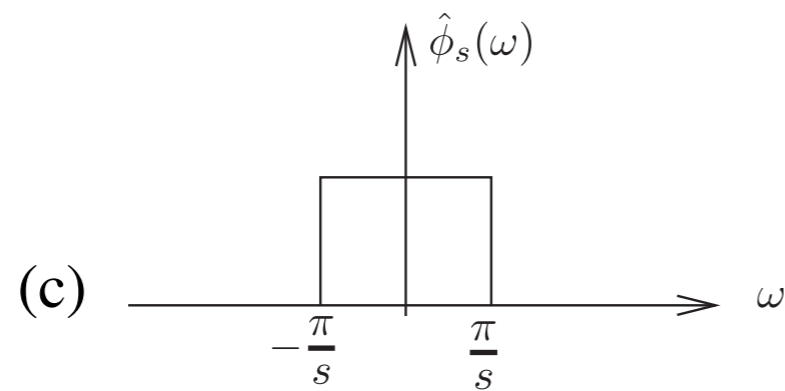
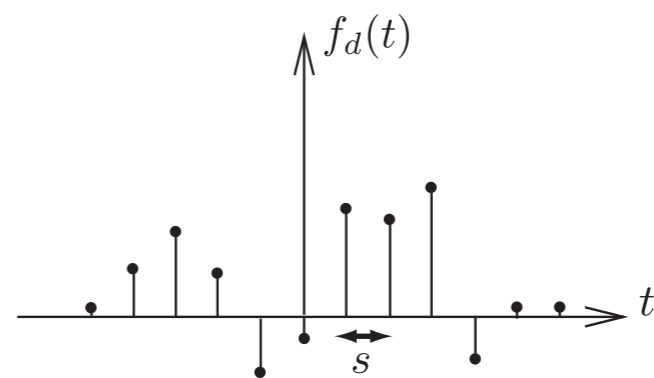
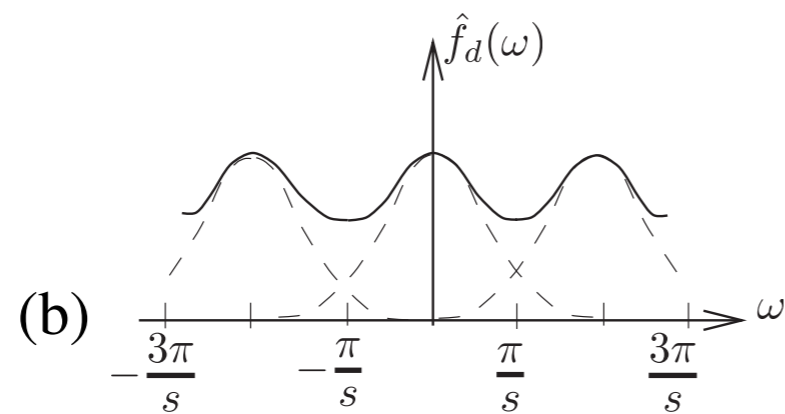
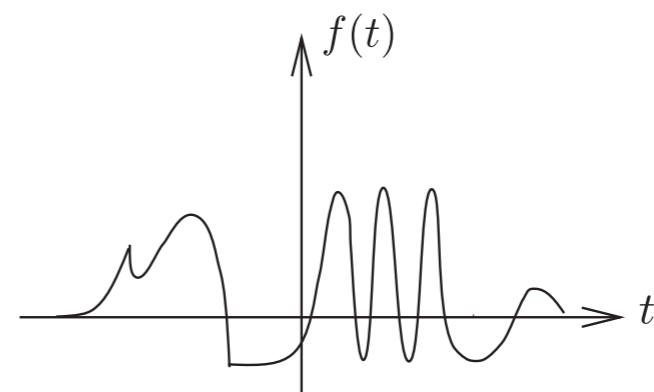
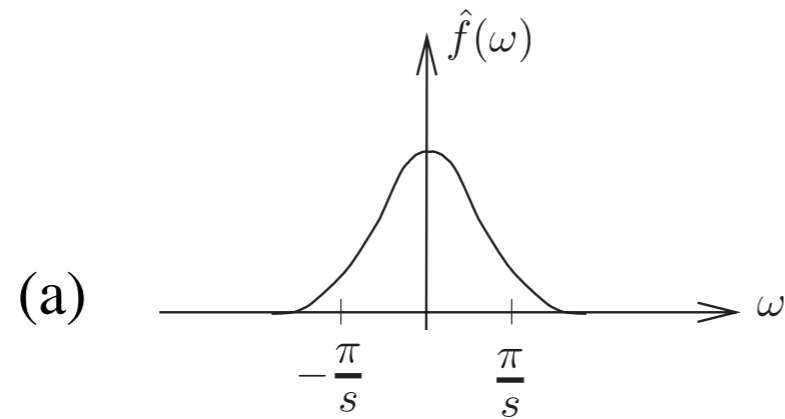
- Natural images are not smooth.
- But can be compressed efficiently.
- Sample *and* compress simultaneously?



Sampling and Periodization



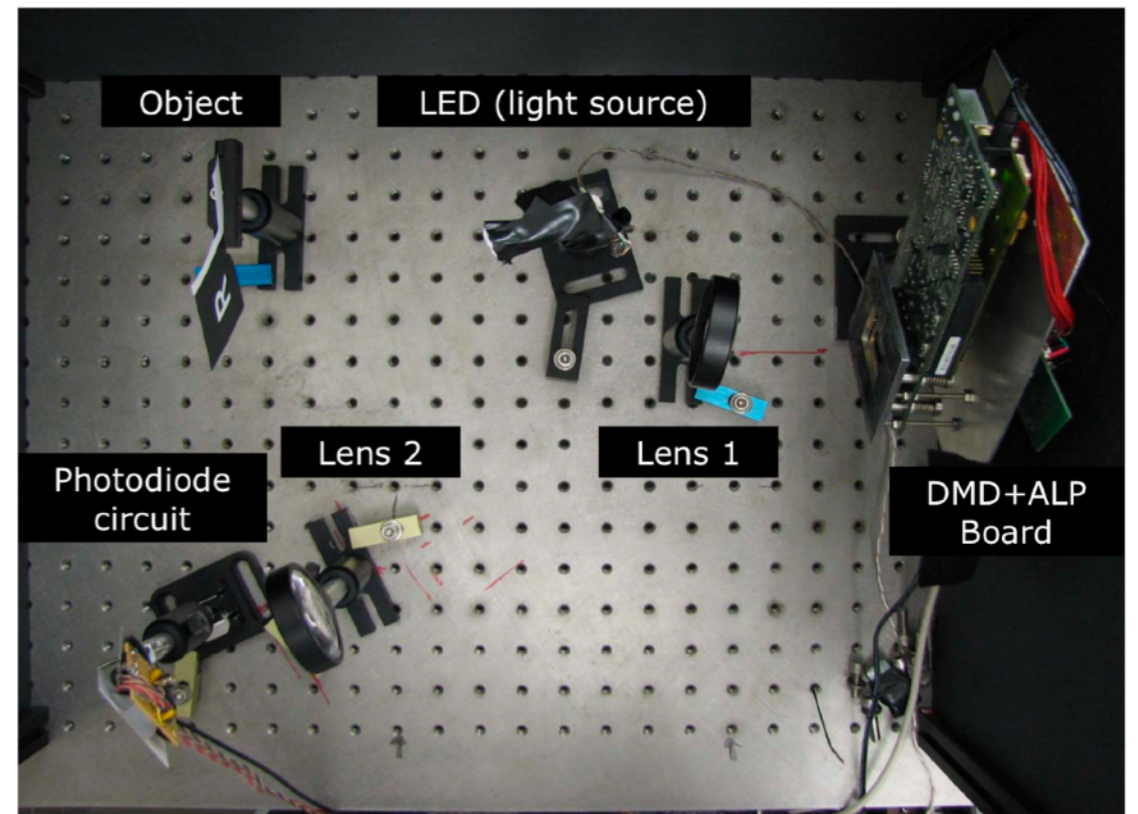
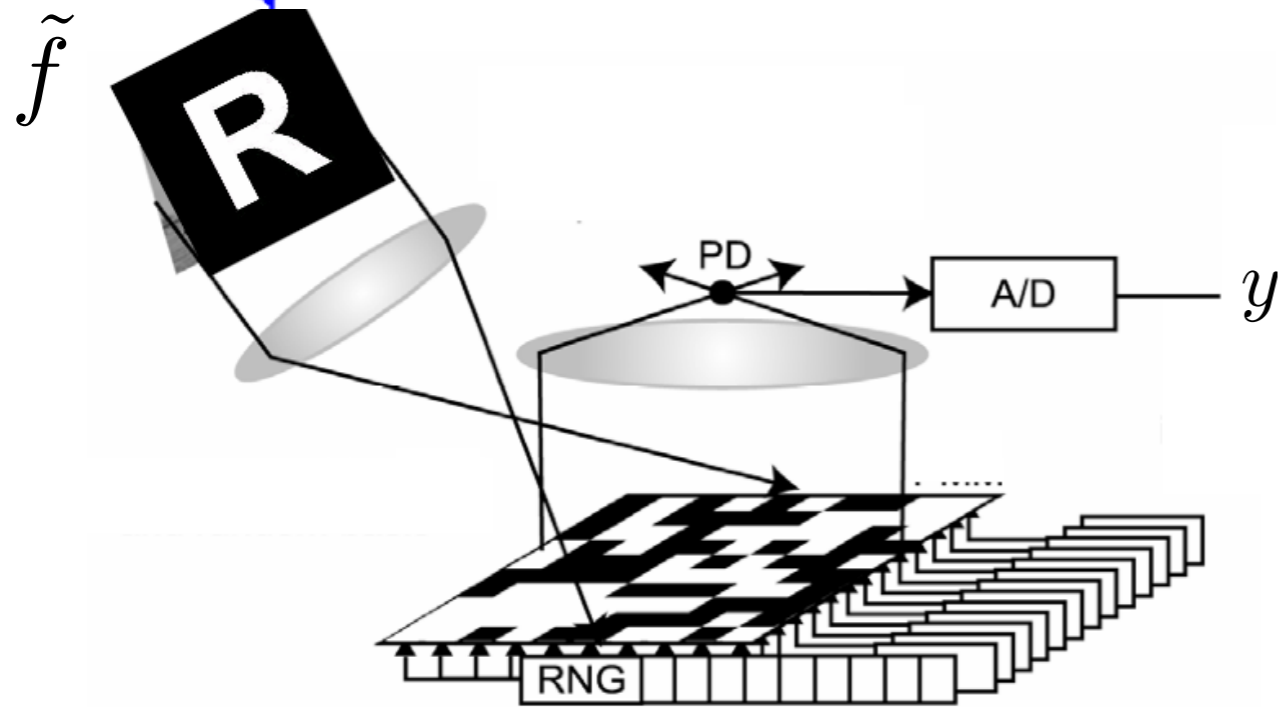
Sampling and Periodization: Aliasing



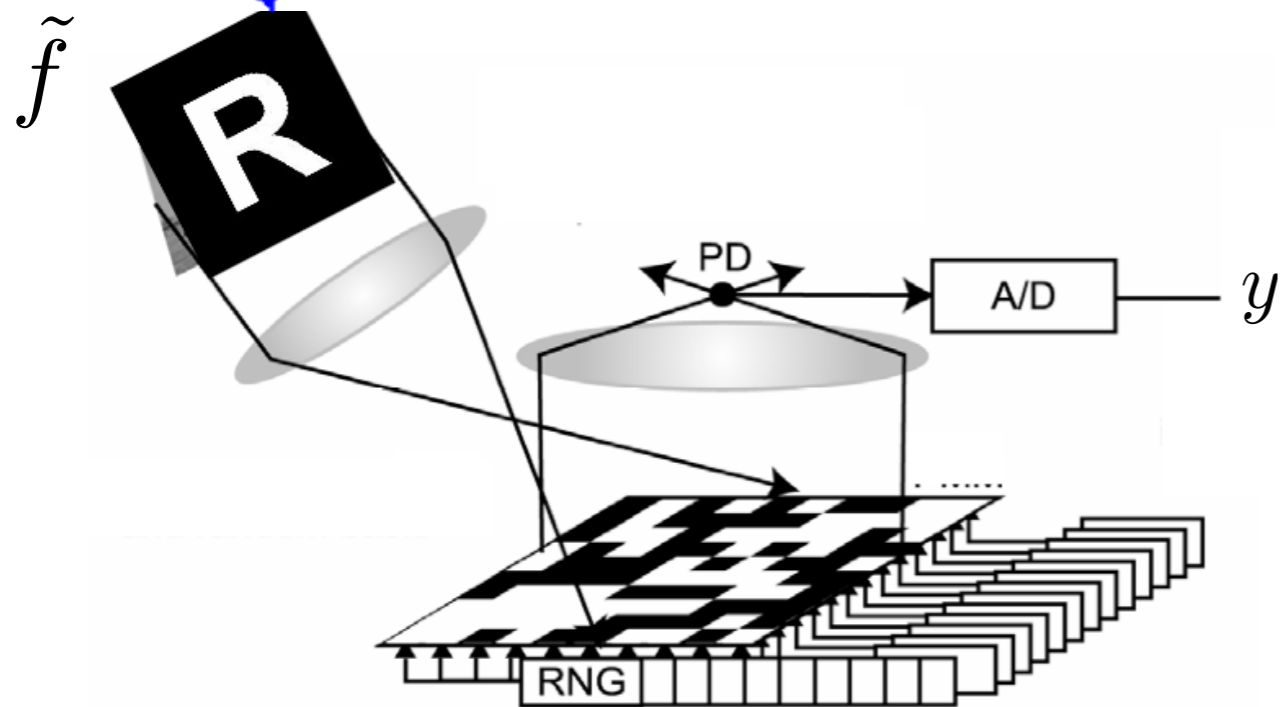
Overview

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- **Compressive Sensing Acquisition**
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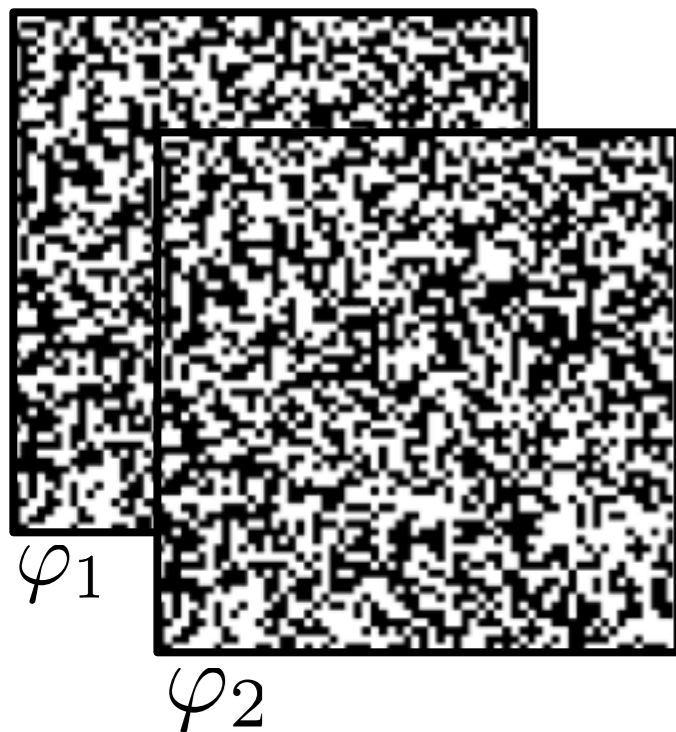
Single Pixel Camera (Rice)



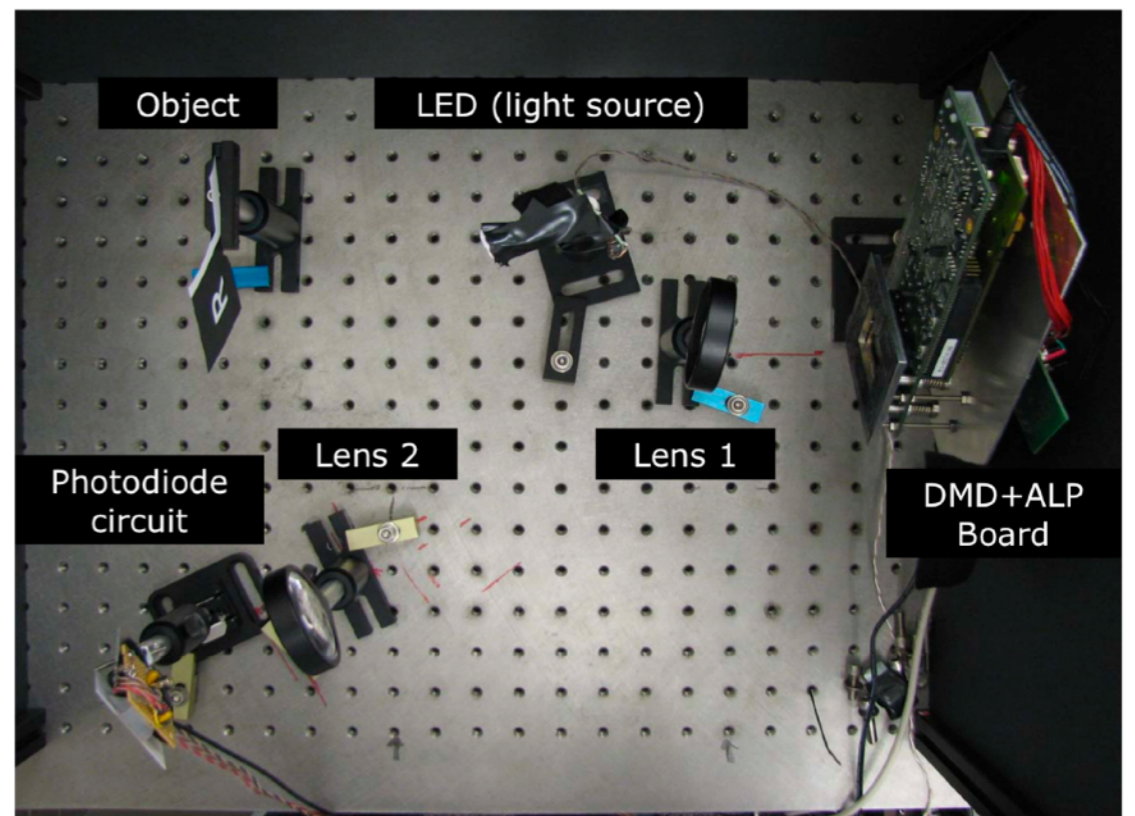
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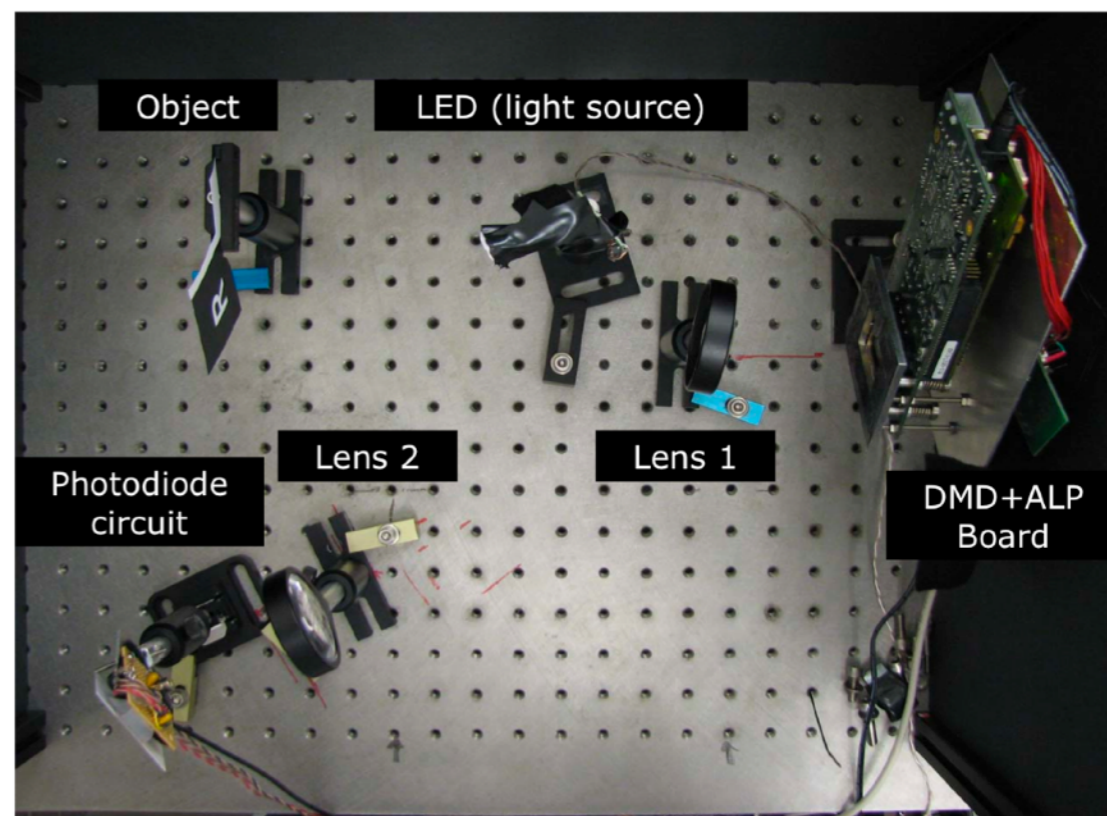
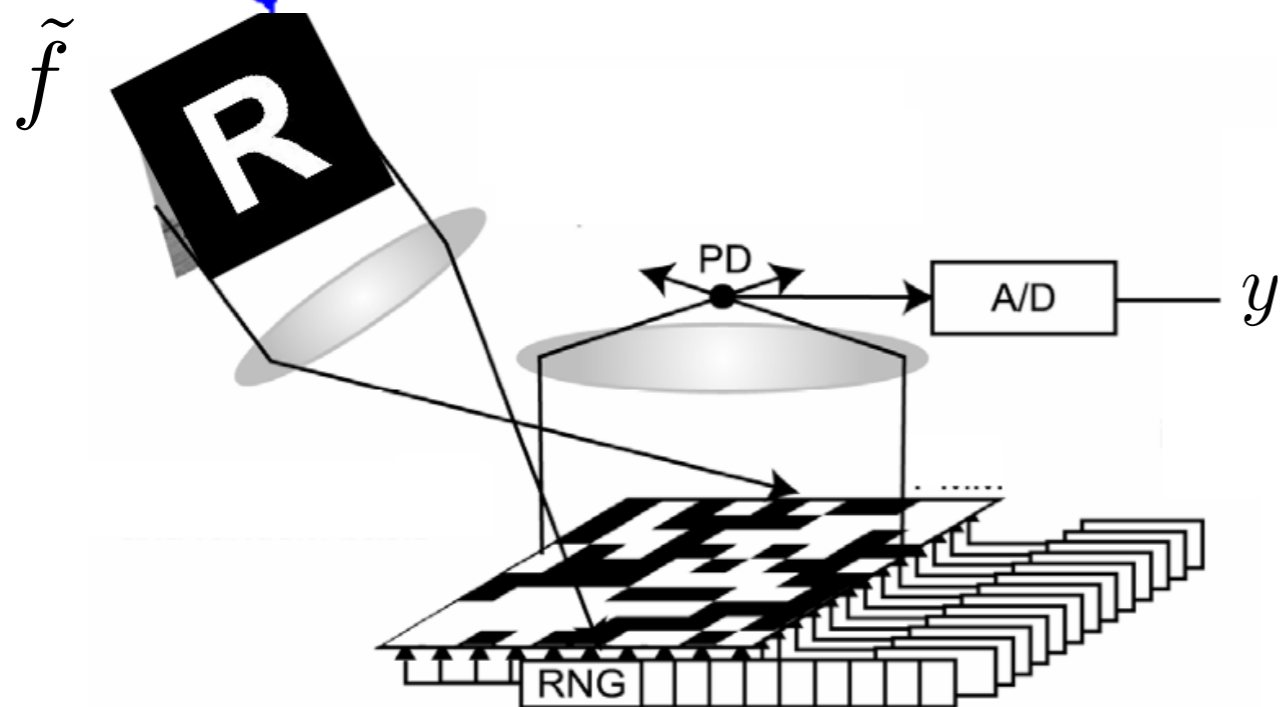
$$y[i] = \langle f, \varphi_i \rangle$$



P measures $\ll N$ micro-mirrors

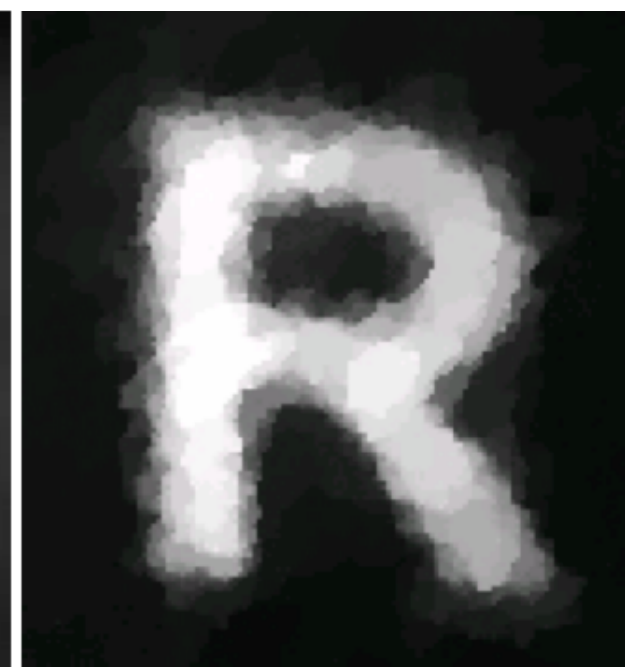
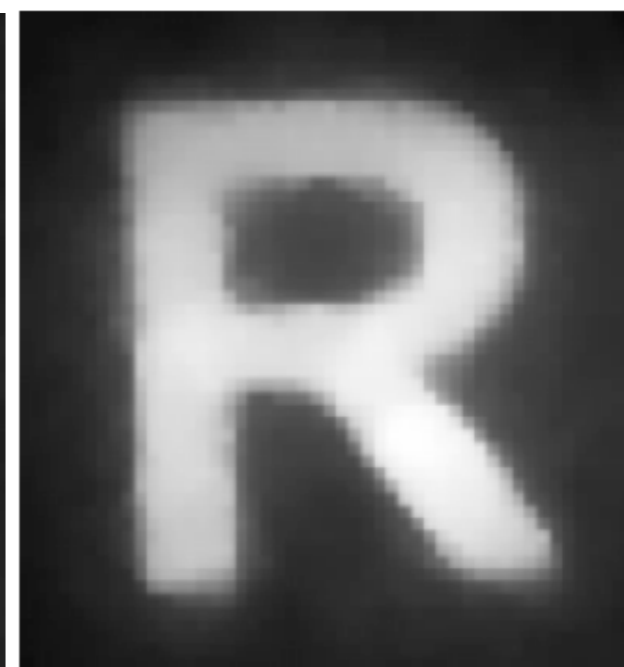
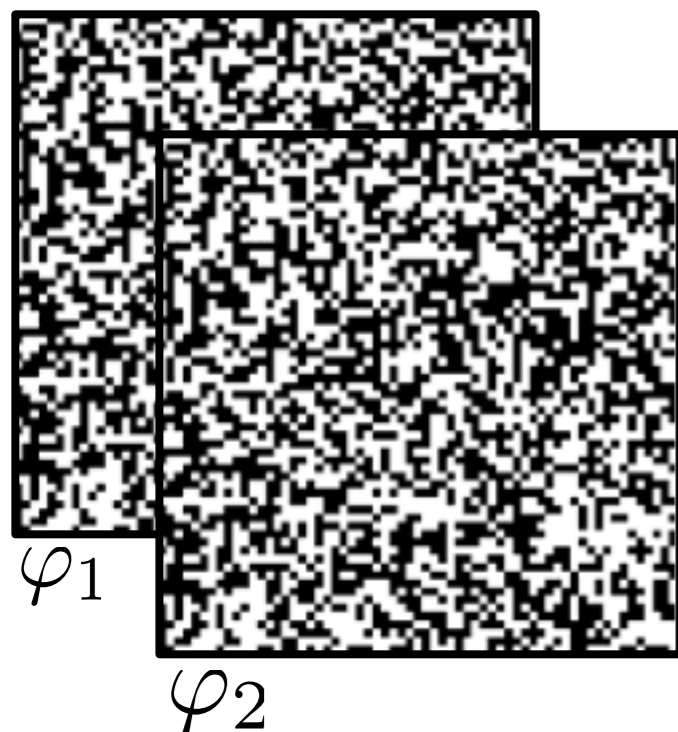


Single Pixel Camera (Rice)



$$y[i] = \langle f, \varphi_i \rangle$$

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$P/N = 1$

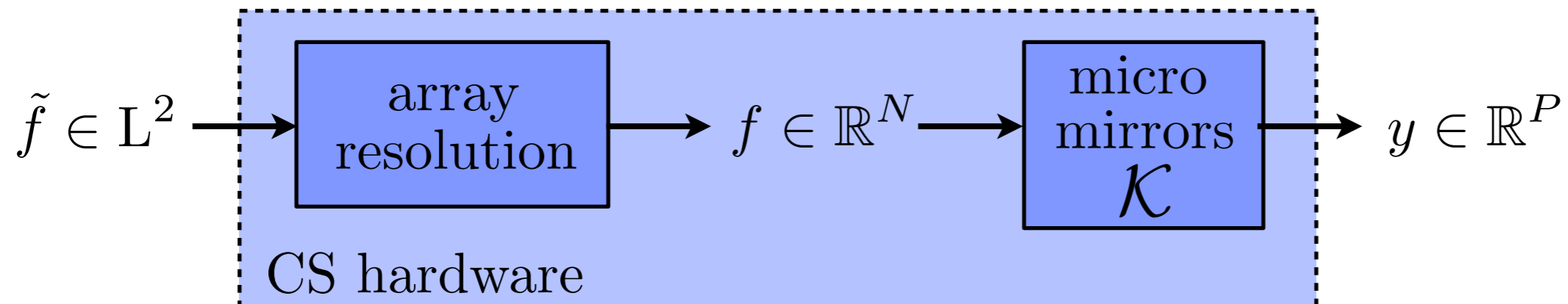
$P/N = 0.16$

$P/N = 0.02$

CS Hardware Model

CS is about designing hardware: input signals $\tilde{f} \in L^2(\mathbb{R}^2)$.

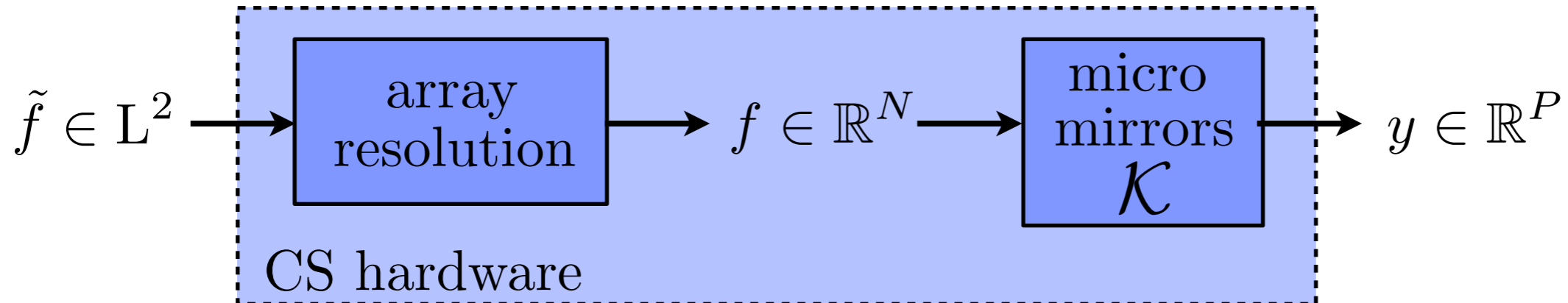
Physical hardware resolution limit: target resolution $f \in \mathbb{R}^N$.



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$$y[0] = \left\langle \begin{array}{c} \text{Lena image} \\ \text{random mask} \end{array}, \right\rangle$$

$$y[1] = \left\langle \begin{array}{c} \text{Lena image} \\ \text{random mask} \end{array}, \right\rangle$$

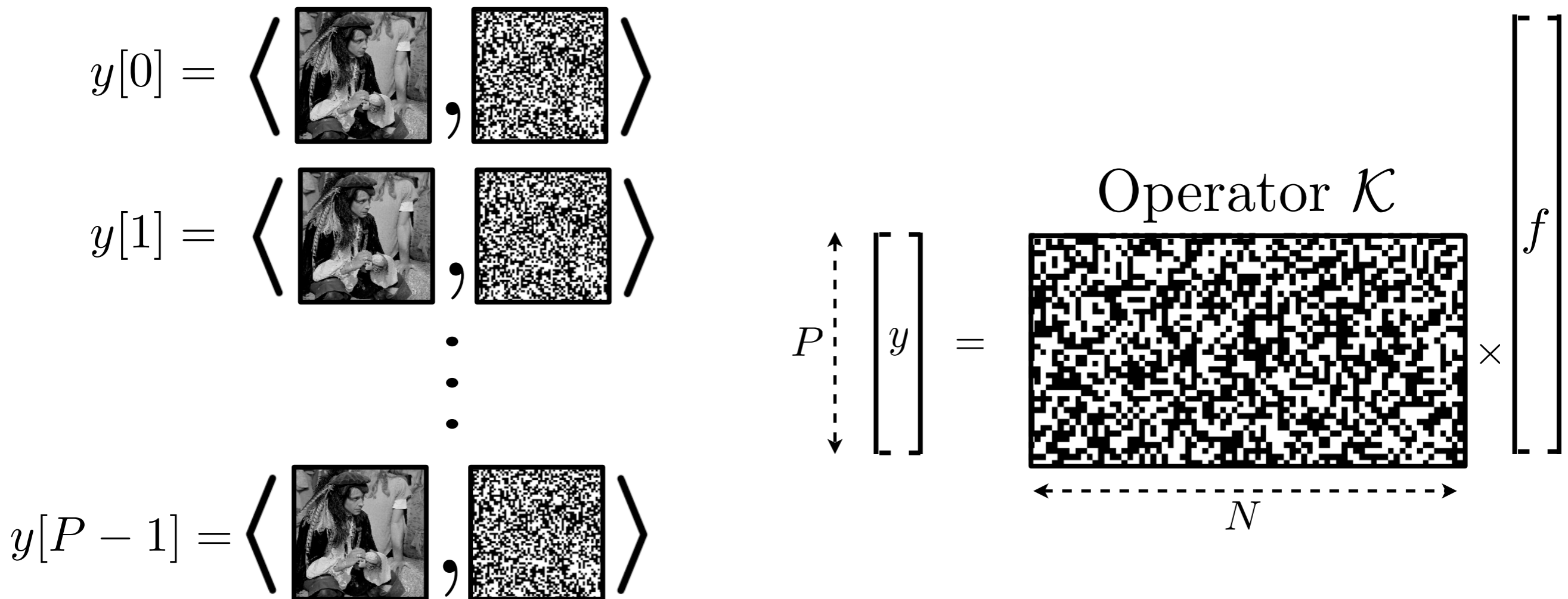
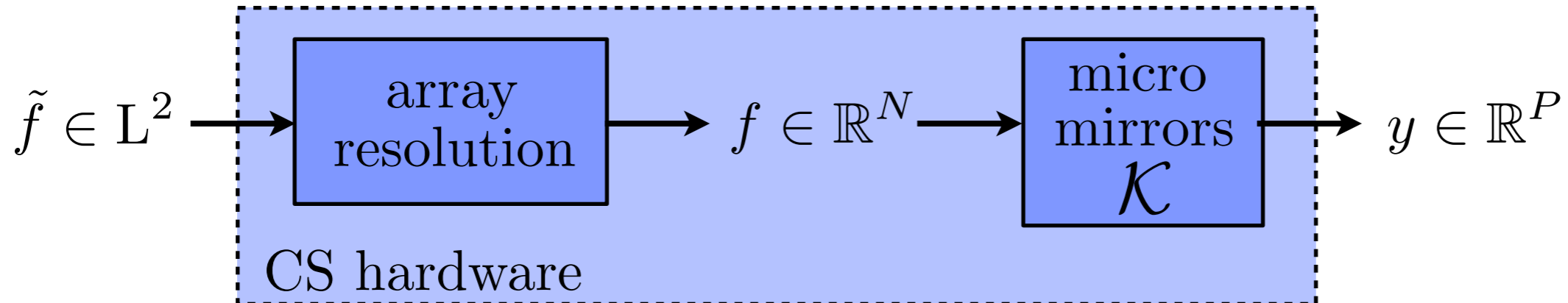
⋮

$$y[P - 1] = \left\langle \begin{array}{c} \text{Lena image} \\ \text{random mask} \end{array}, \right\rangle$$

CS Hardware Model

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Physical hardware resolution limit: target resolution $f \in \mathbb{R}^N$.



Overview

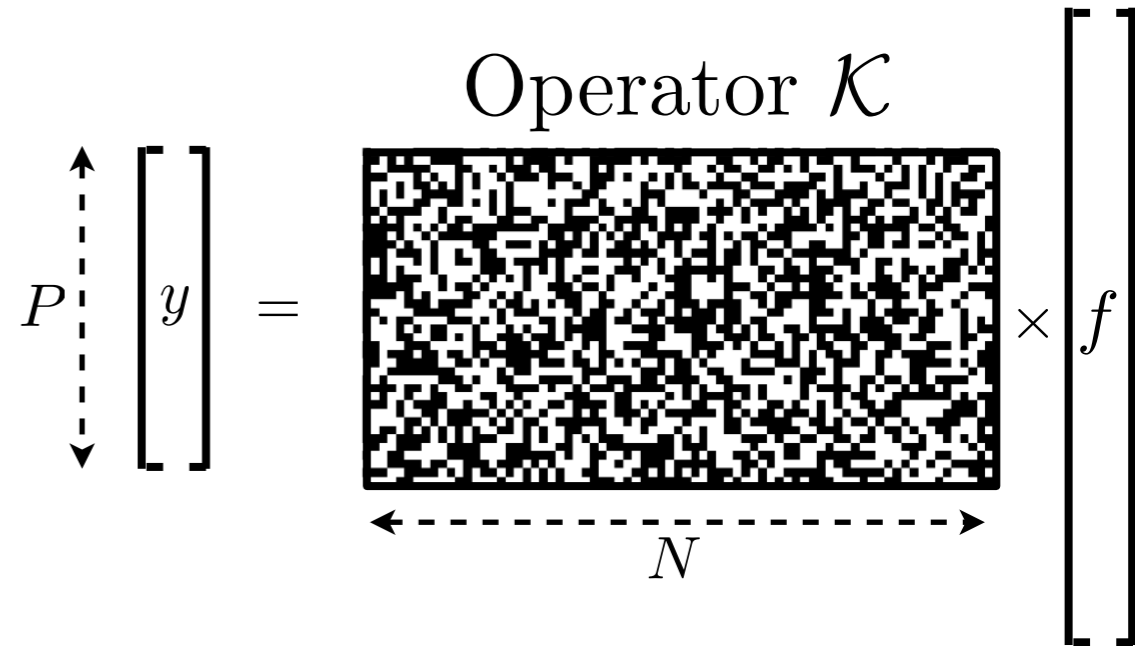
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Inversion and Sparsity

Need to solve $y = \mathcal{K}f$.

→ More unknown than equations.

$\dim(\ker(\mathcal{K})) = N - P$ is huge.

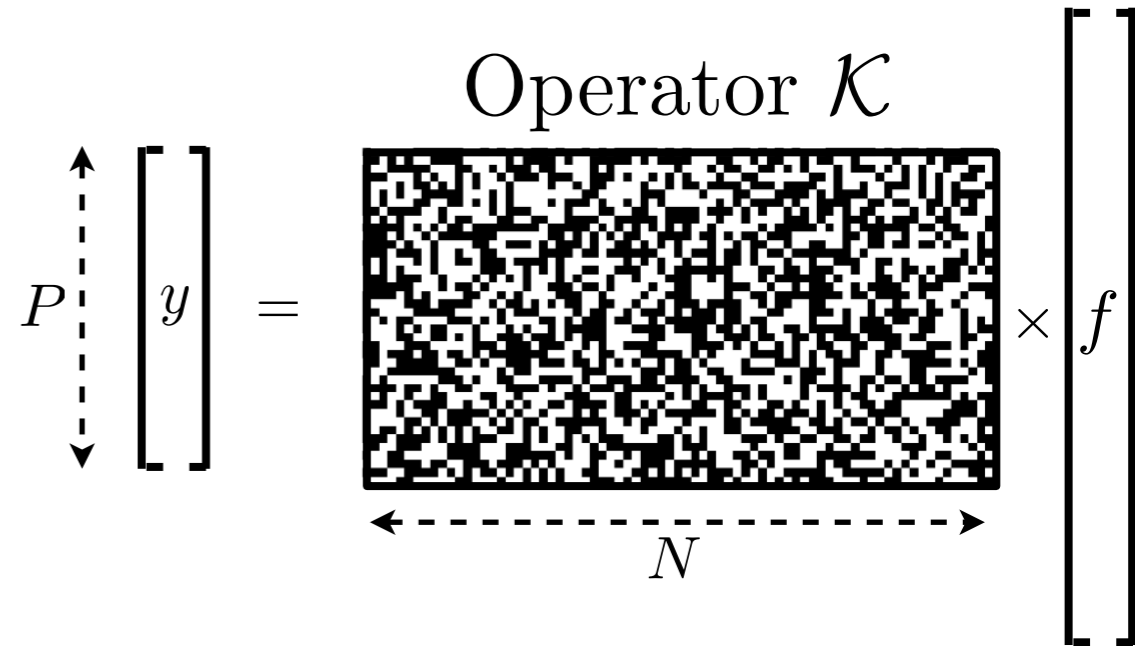


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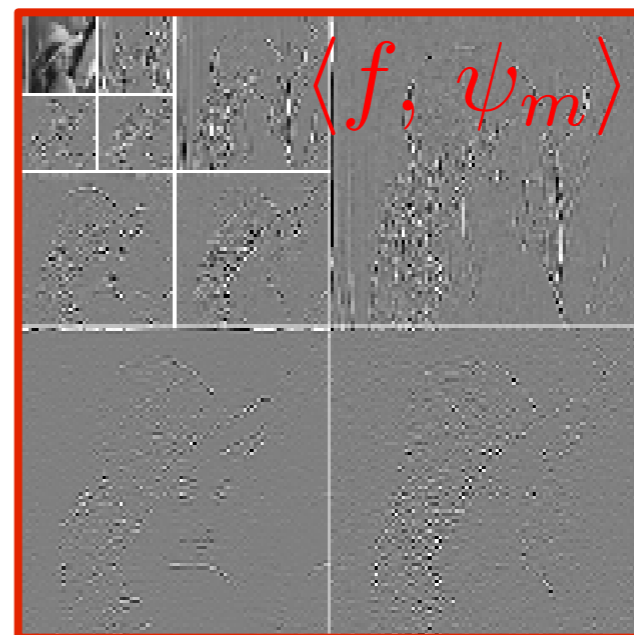
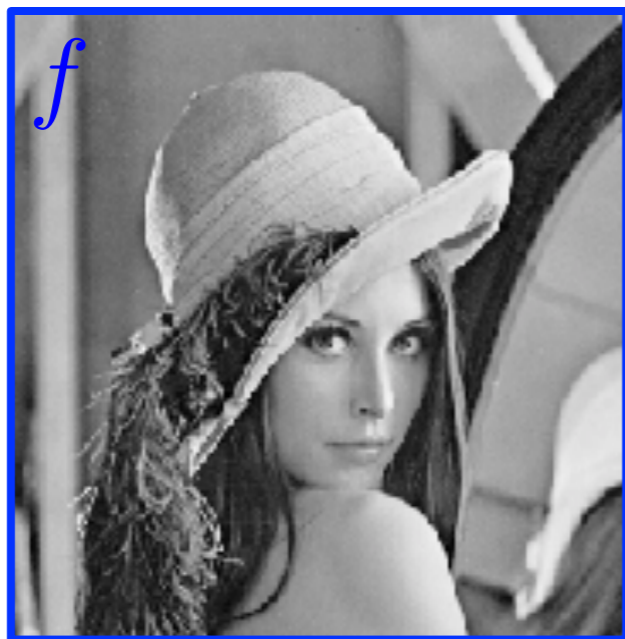
→ More unknown than equations.

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Prior information: f is sparse in a basis $\{\psi_m\}_m$.

$J_\varepsilon(f) = \text{Card} \{m \mid |\langle f, \psi_m \rangle| > \varepsilon\}$ is small.



Convex Relaxation: L1 Prior

“Ideal” sparsity prior:

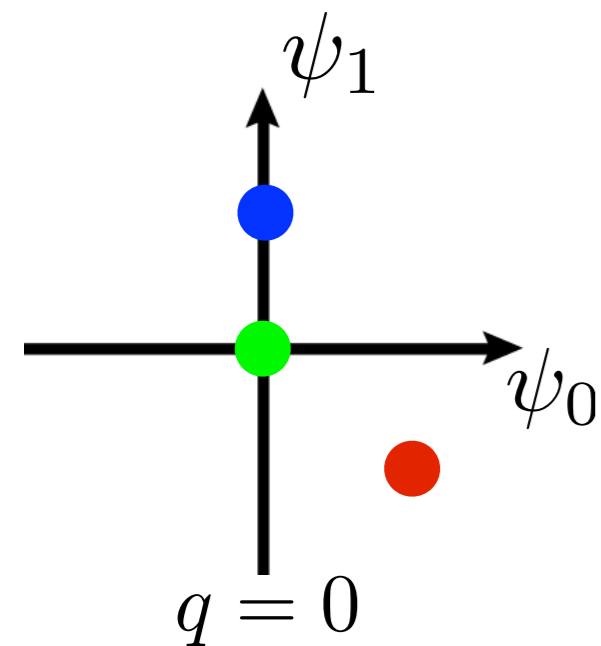
$$J_0(f) = \# \{m \mid \langle f, \psi_m \rangle \neq 0\}$$

Image with 2 pixels:

$J_0(f) = 0$ \longrightarrow null image. ●

$J_0(f) = 1$ \longrightarrow sparse image. ●

$J_0(f) = 2$ \longrightarrow non-sparse image. ●



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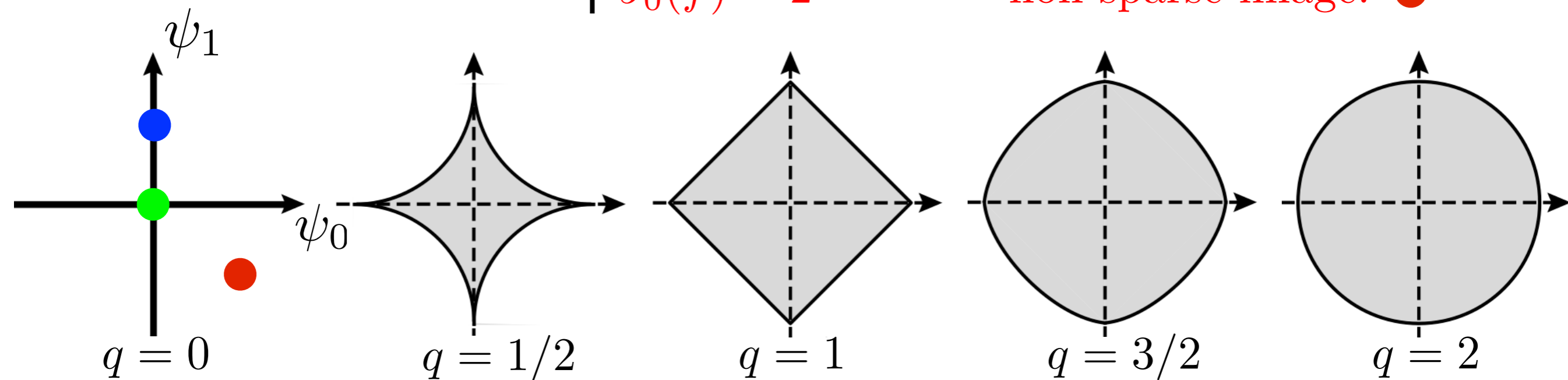
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ℓ^q priors:

$$J_q(f) = \sum_m |\langle f, \psi_m \rangle|^q$$

(convex for $q \geq 1$)

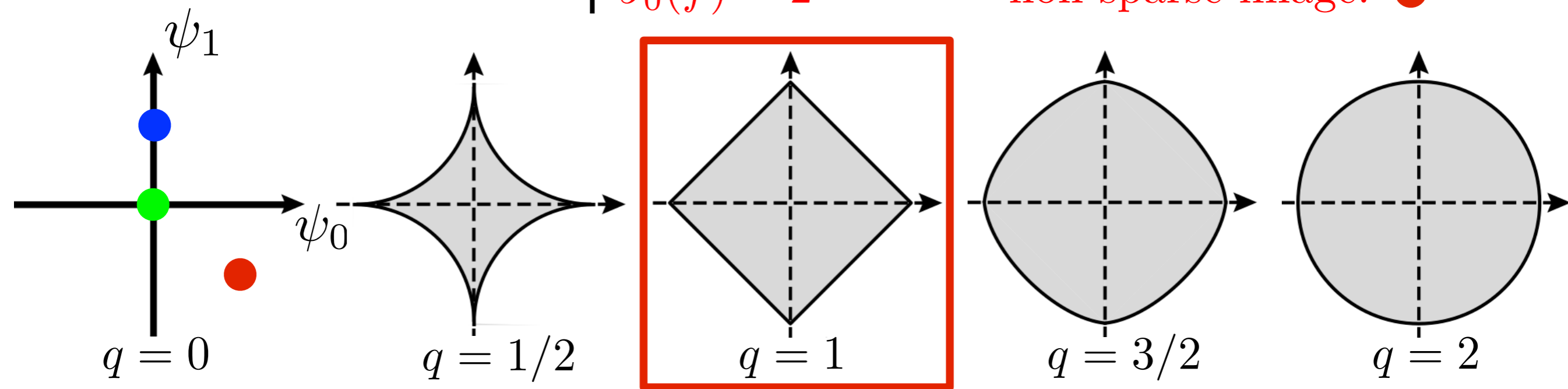
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ℓ^q priors:

$$J_q(f) = \sum_m |\langle f, \psi_m \rangle|^q \quad (\text{convex for } q \geq 1)$$

ℓ^1 norm: ℓ^q norm the “closest” to the ℓ^0 ideal sparsity.

Sparse ℓ^1 prior:

$$J_1(f) = \sum_m |\langle f, \psi_m \rangle|$$

Sparse CS Recovery

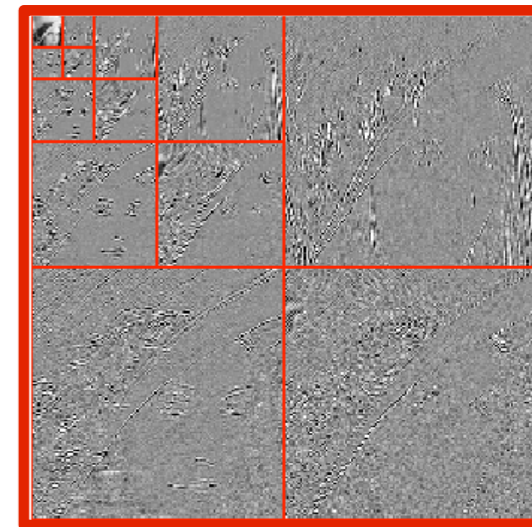
$f_0 \in \mathbb{R}^N$ sparse in ortho-basis Ψ

$$f_0 \in \mathbb{R}^N$$



$$\Psi^*$$

$$\Psi$$



$$x_0 \in \mathbb{R}^N$$

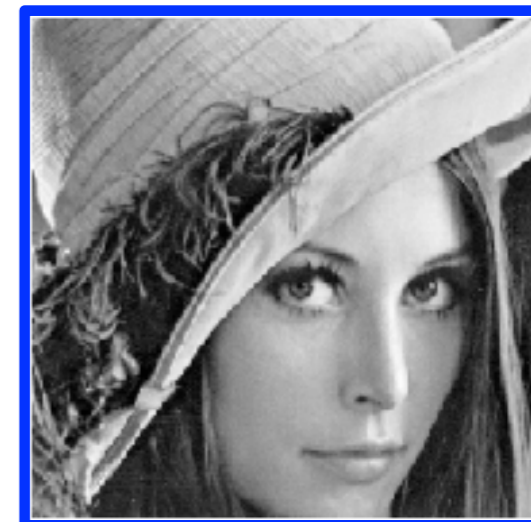
Sparse CS Recovery

$f_0 \in \mathbb{R}^N$ sparse in ortho-basis Ψ

(Discretized) sampling acquisition:

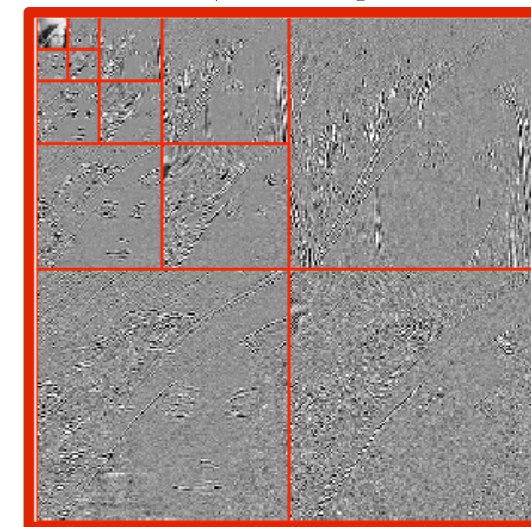
$$y = \mathcal{K} f_0 + w = \mathcal{K} \circ \Psi(x_0) + w \\ = \Phi$$

$$f_0 \in \mathbb{R}^N$$



Ψ^*

Ψ



$$x_0 \in \mathbb{R}^N$$

Sparse CS Recovery

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\mathcal{K} drawn from the Gaussian matrix ensemble

$$\mathcal{K}_{i,j} \sim \mathcal{N}(0, P^{-1/2}) \text{ i.i.d.}$$

$\Rightarrow \Phi$ drawn from the Gaussian matrix ensemble

$$f_0 \in \mathbb{R}^N$$



$$\Psi^* \downarrow \quad \uparrow \Psi$$



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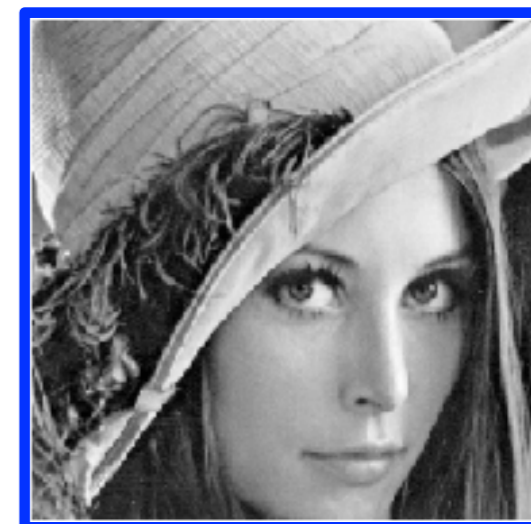
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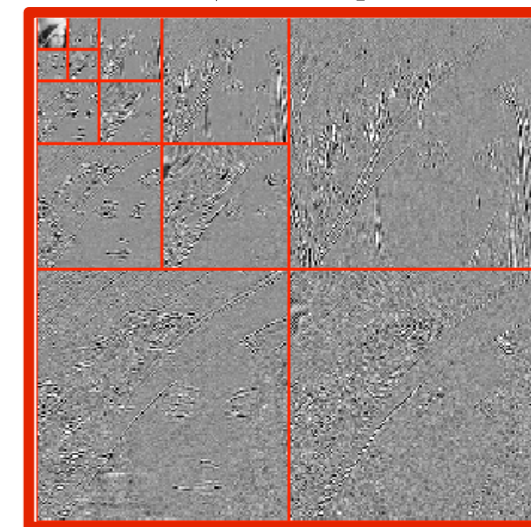
Sparse recovery:

$$\min_{\|\Phi x - y\| \leq \|w\|} \|x\|_1 \quad \xleftrightarrow{\|w\| \longleftrightarrow \lambda} \quad \min_x \frac{1}{2} \|\Phi x - y\|^2 + \lambda \|x\|_1$$

$$f_0 \in \mathbb{R}^N$$

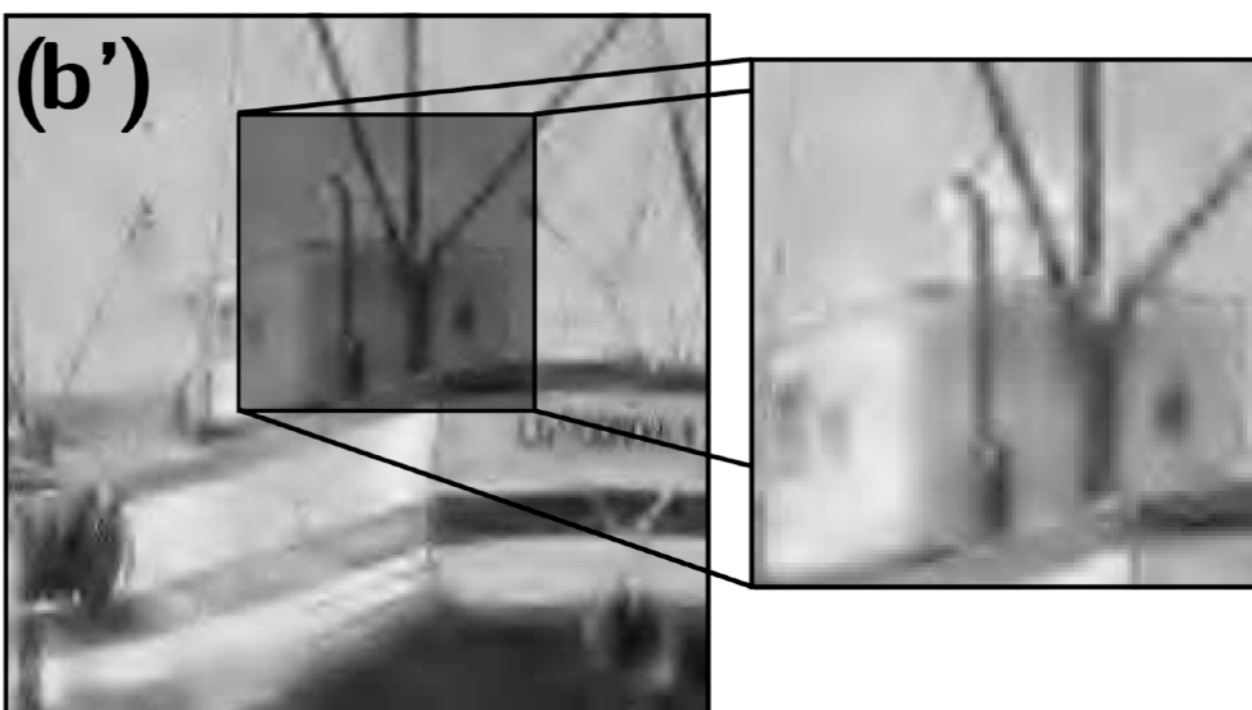
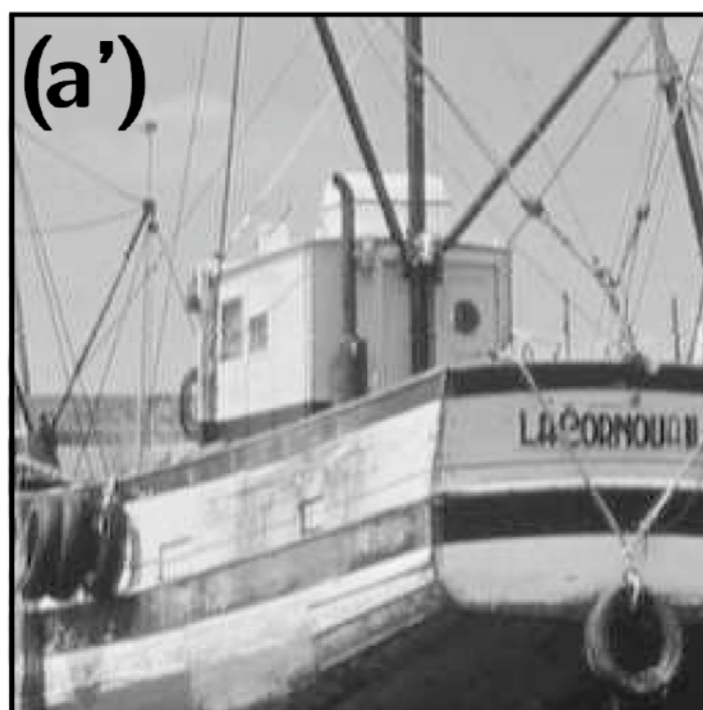
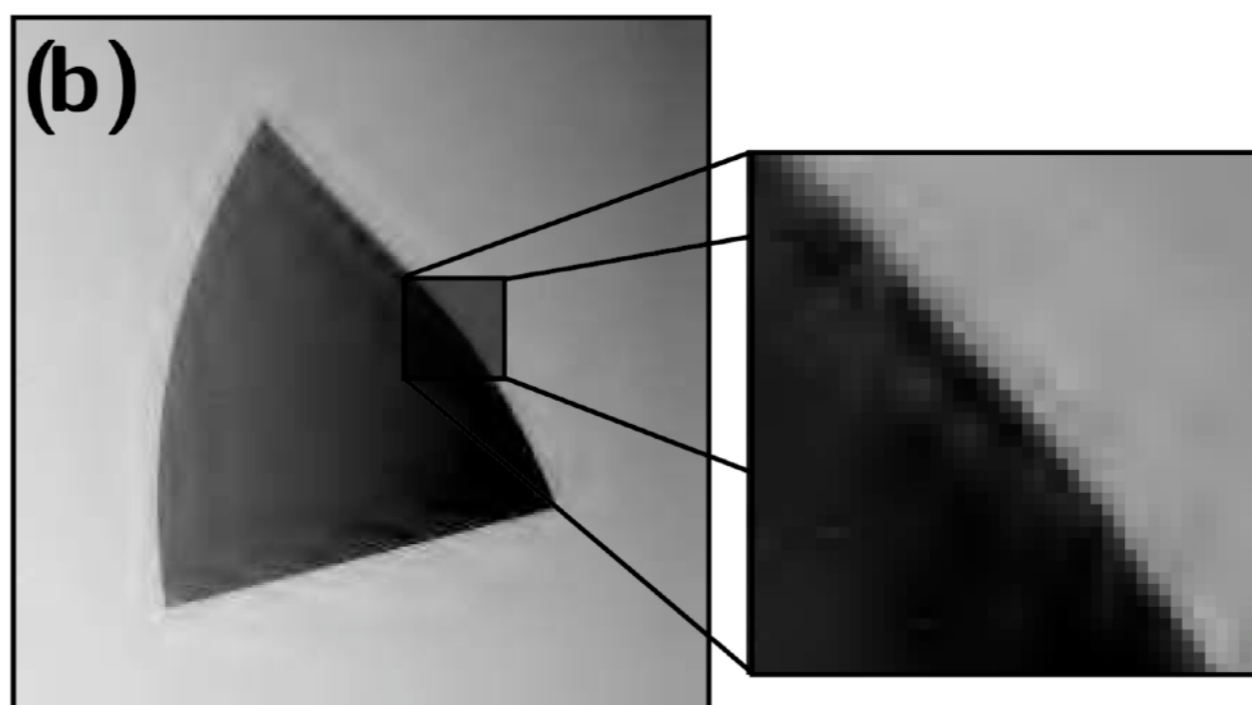
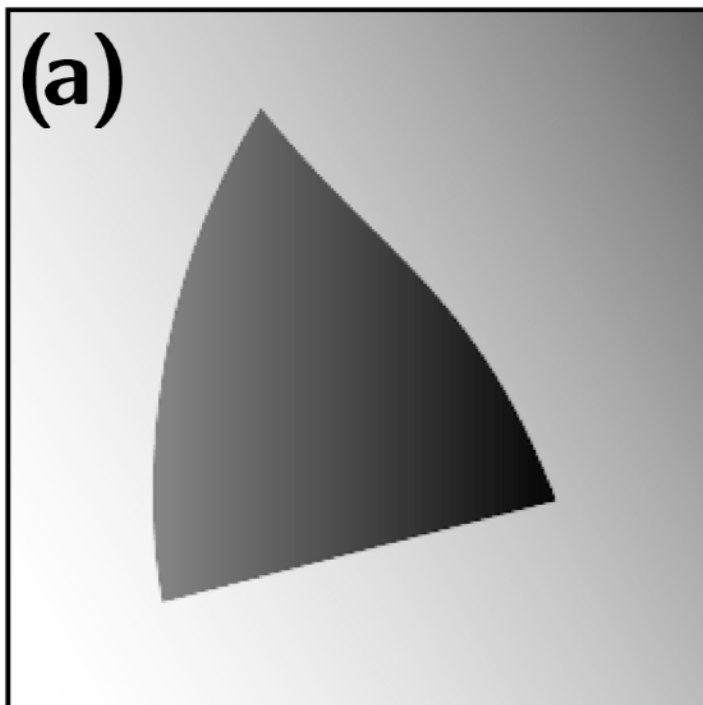


$$\Psi^* \downarrow \quad \uparrow \Psi$$



$$x_0 \in \mathbb{R}^N$$

CS Simulation Example



Original f_0

Recovery f^* , $P = N/6$

$\Psi =$ translation invariant
wavelet frame

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CS with RIP

ℓ^1 recovery:

$$x^* \in \underset{\|\Phi x - y\| \leq \varepsilon}{\operatorname{argmin}} \|x\|_1 \quad \text{where} \quad \begin{cases} y = \Phi x_0 + w \\ \|w\| \leq \varepsilon \end{cases}$$

Restricted Isometry Constants:

$$\forall \|x\|_0 \leq k, \quad (1 - \delta_k) \|x\|^2 \leq \|\Phi x\|^2 \leq (1 + \delta_k) \|x\|^2$$

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Restricted Isometry Constants:

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Theorem: If $\delta_{2k} \leq \sqrt{2} - 1$, then [Candes 2009]

$$\|x_0 - x^*\| \leq \frac{C_0}{\sqrt{k}} \|x_0 - x_k\|_1 + C_1 \varepsilon$$

where x_k is the best k -term approximation of x_0 .

RIP for Gaussian Matrices

Link with coherence: $\mu(\Phi) = \max_{i \neq j} |\langle \varphi_i, \varphi_j \rangle|$

$$\delta_2 = \mu(\Phi)$$

$$\delta_k \leq (k - 1)\mu(\Phi)$$

RIP for Gaussian Matrices

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For Gaussian matrices:

$$\mu(\Phi) \sim \sqrt{\log(PN)/P}$$

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Stronger result:

Theorem: If $k \leq \frac{C}{\log(N/P)} P$ [Candès et al, 2004]

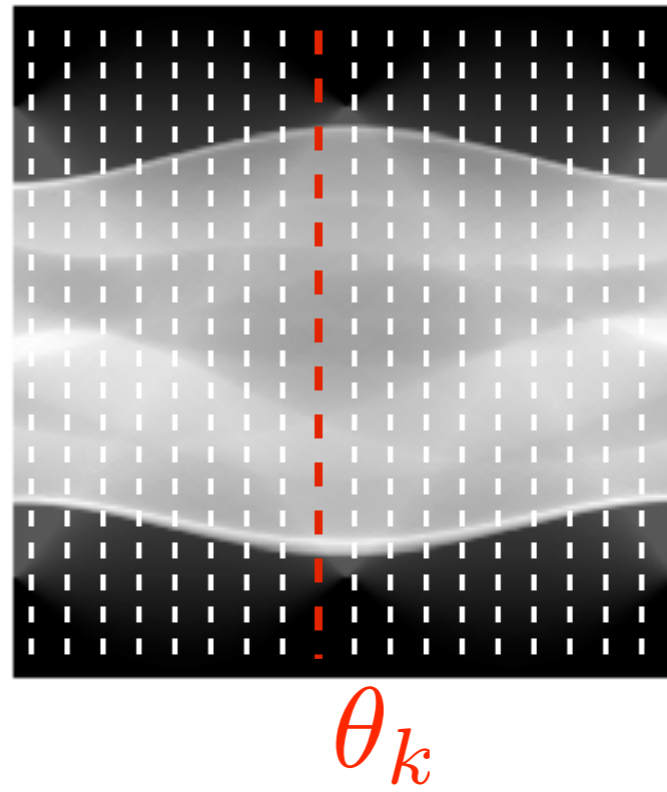
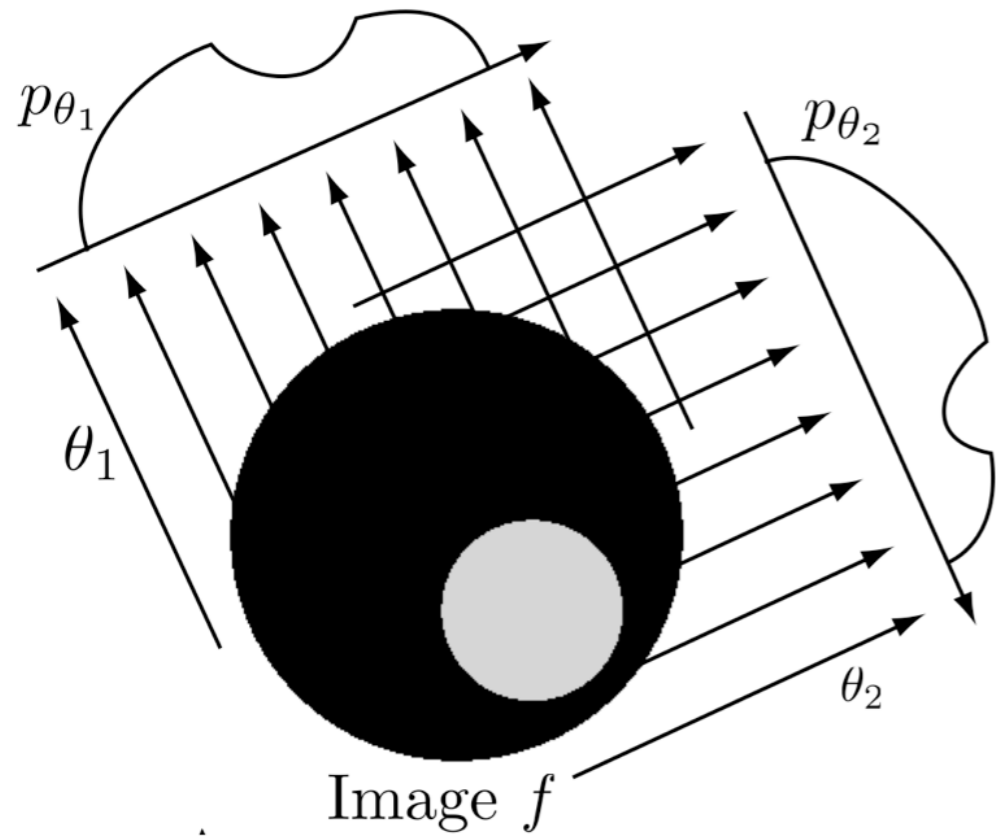
then $\delta_{2k} \leq \sqrt{2} - 1$ with high probability.

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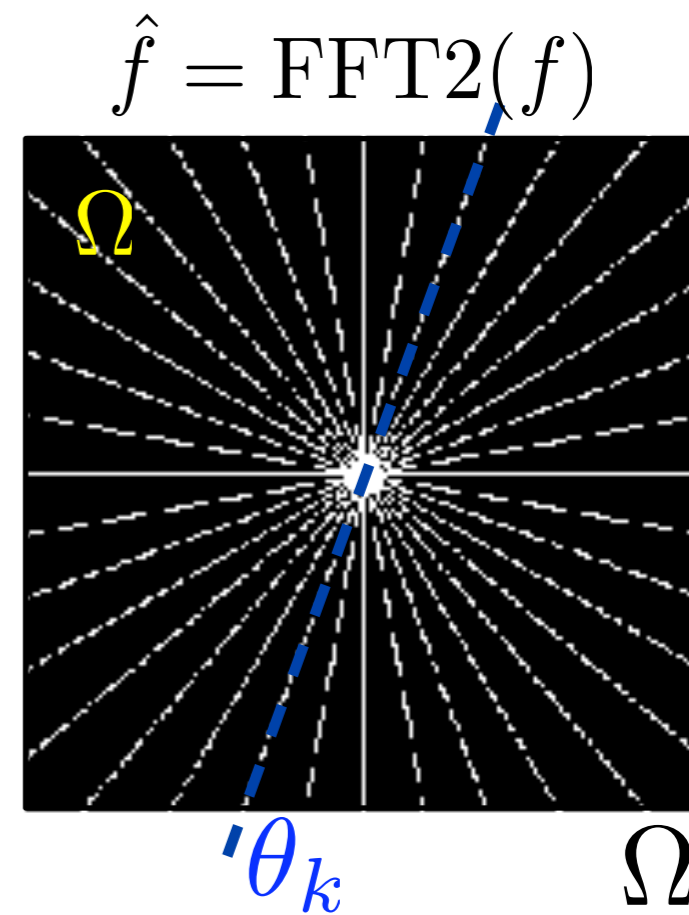
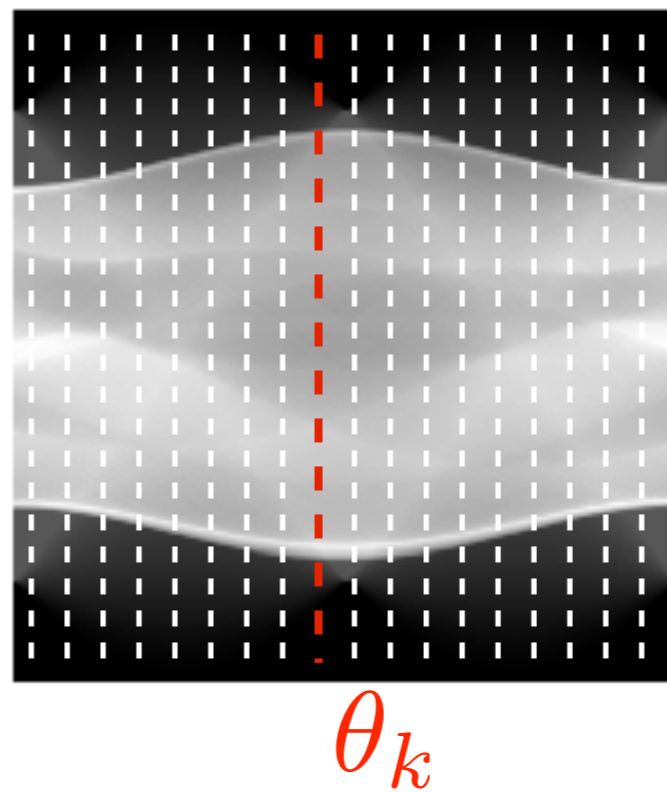
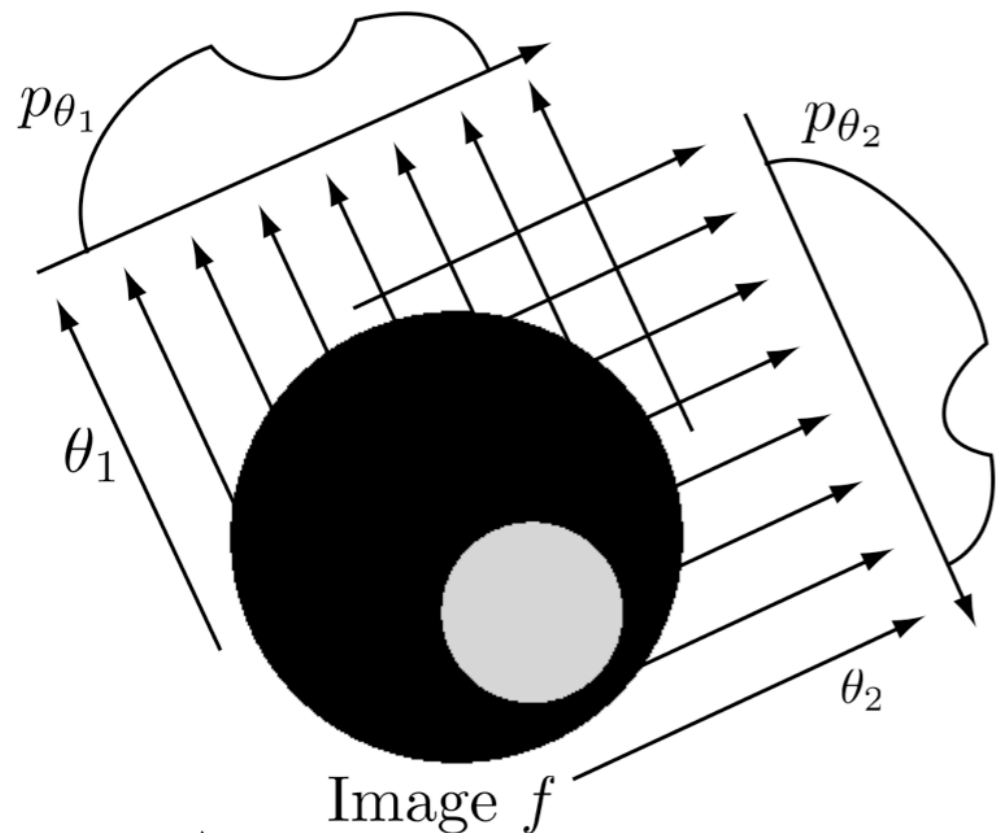
Tomography and Fourier Measures

Tomography projection:



Tomography and Fourier Measures

Tomography projection:



Fourier slice theorem:

$$\underbrace{\hat{p}_\theta(\rho)}_{\text{1D}} = \underbrace{\hat{f}(\rho \cos(\theta), \rho \sin(\theta))}_{\text{2D Fourier}}$$

Partial Fourier measurements: $\{p_{\theta_k}(t)\}_{0 \leq k < K}^{t \in \mathbb{R}}$

Equivalent to: $\mathcal{K}f = (\hat{f}[\omega])_{\omega \in \Omega}$

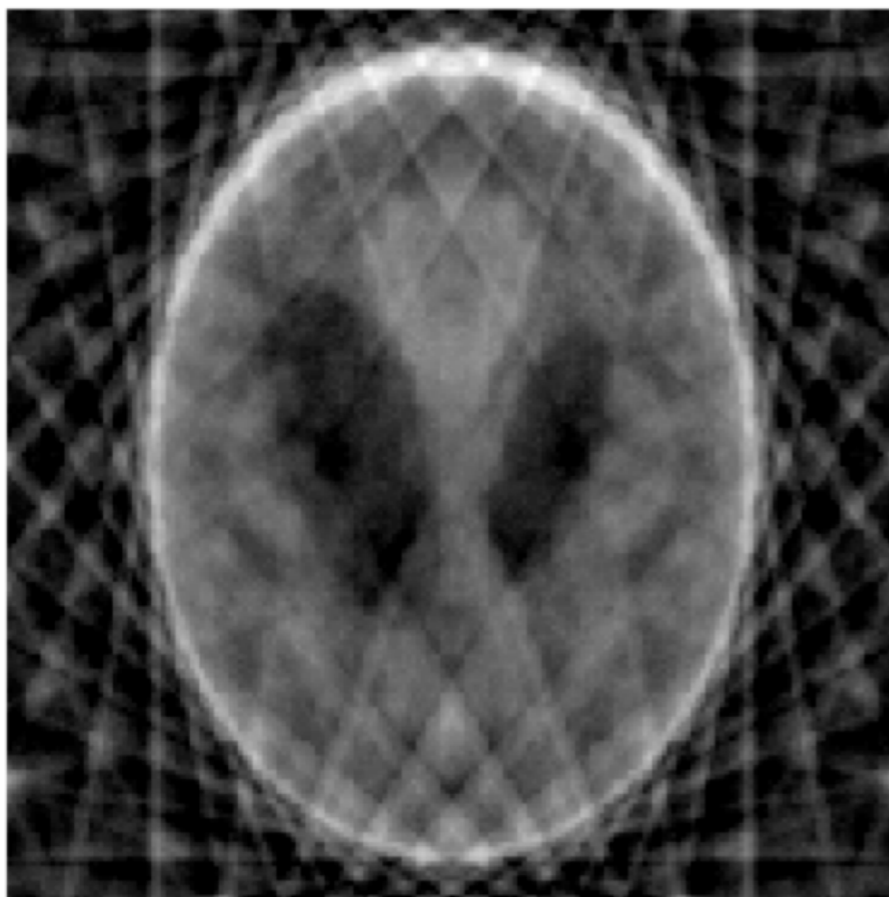
Regularized Inversion

Noisy measurements: $\forall \omega \in \Omega, y[\omega] = \hat{f}_0[\omega] + w[\omega]$.

Noise: $w[\omega] \sim \mathcal{N}(0, \sigma)$, white noise.

ℓ^1 regularization:

$$f^* = \operatorname{argmin}_f \frac{1}{2} \sum_{\omega \in \Omega} |y[\omega] - \hat{f}[\omega]|^2 + \lambda \sum_m |\langle f, \psi_m \rangle|.$$



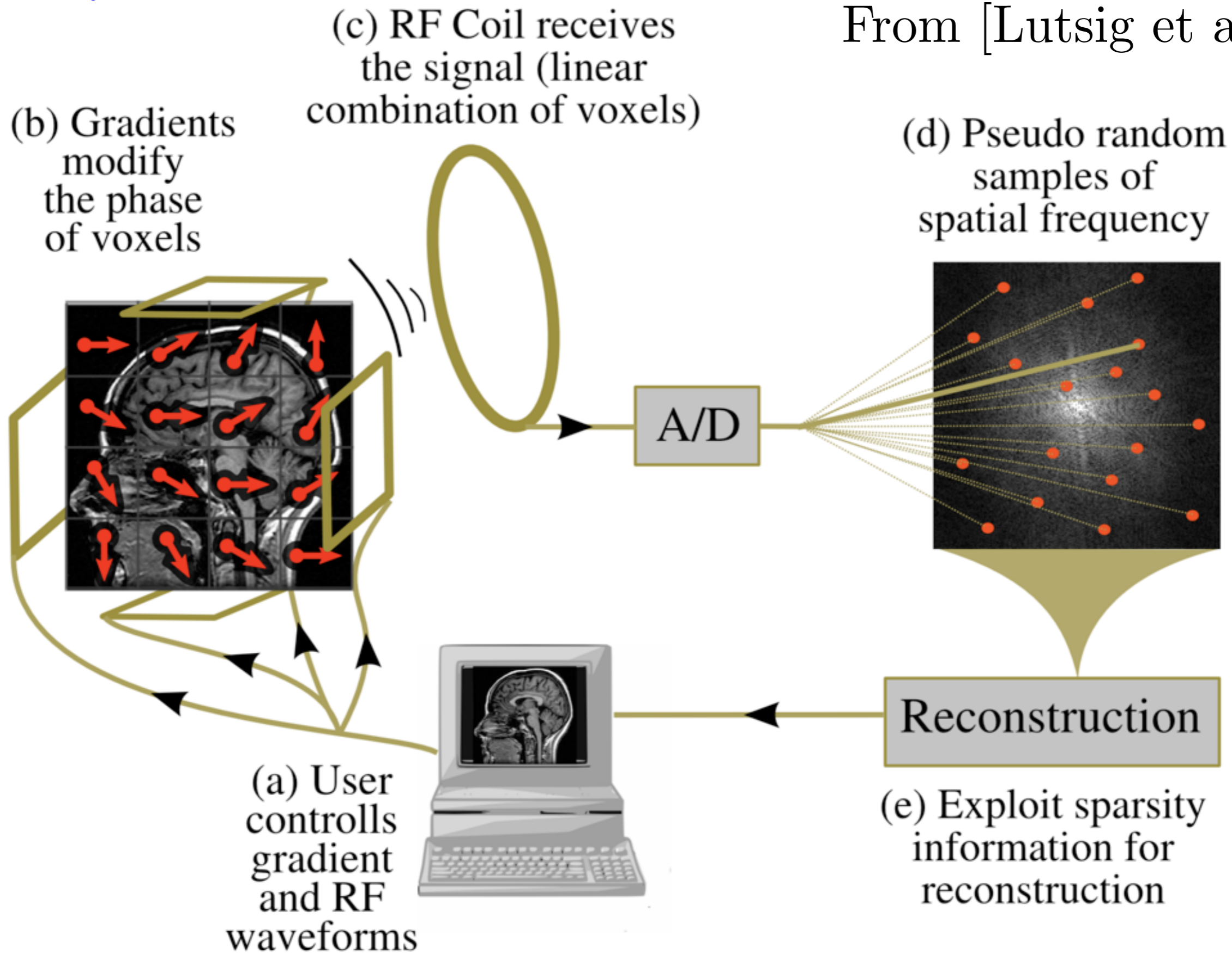
f^+



f^*

MRI Imaging

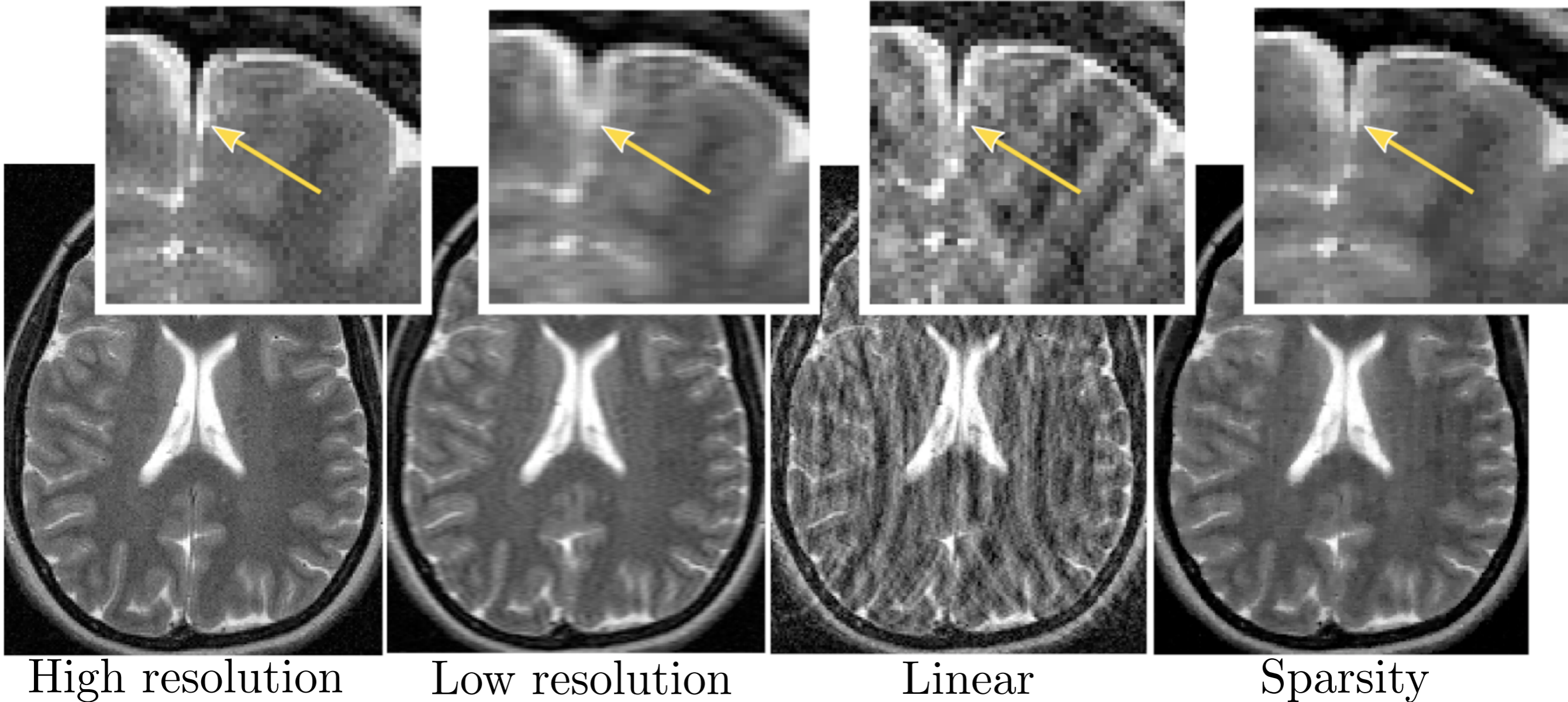
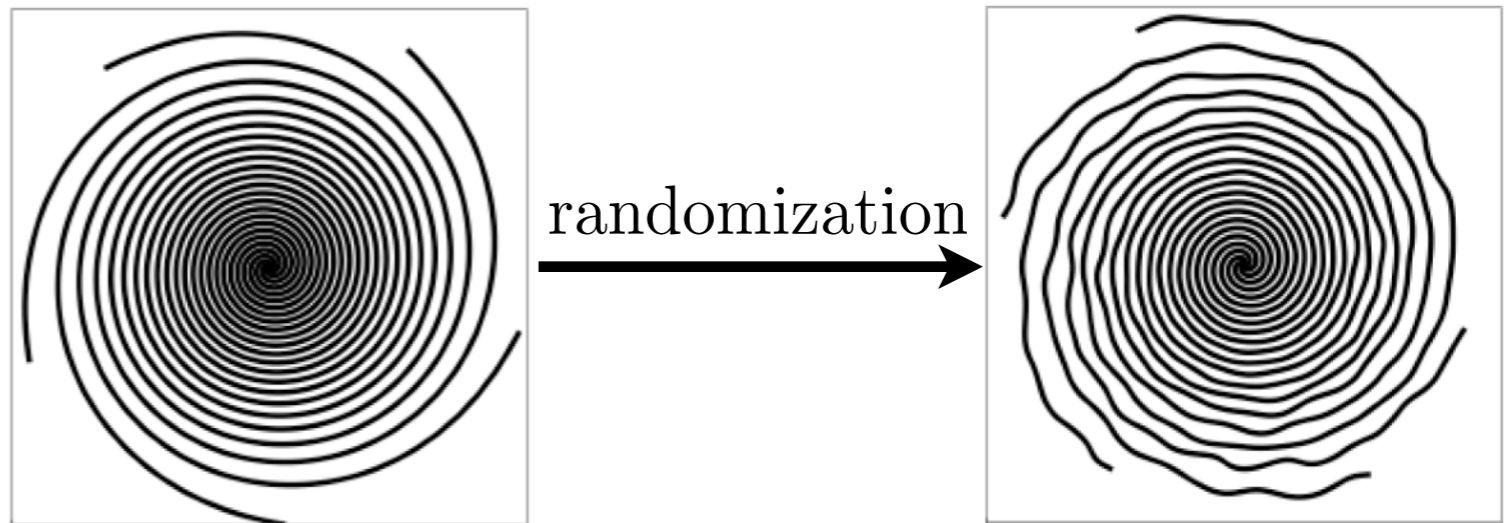
From [Lutsig et al.]



MRI Reconstruction

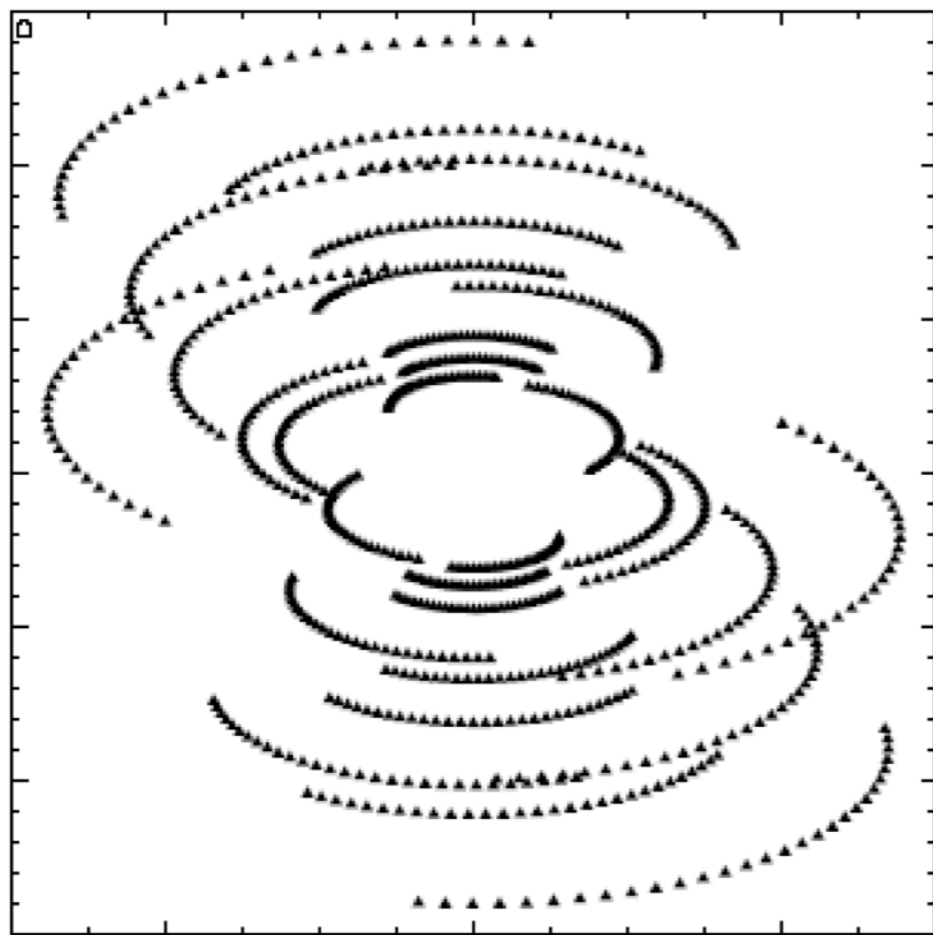
From [Lutsig et al.]

Fourier sub-sampling pattern:

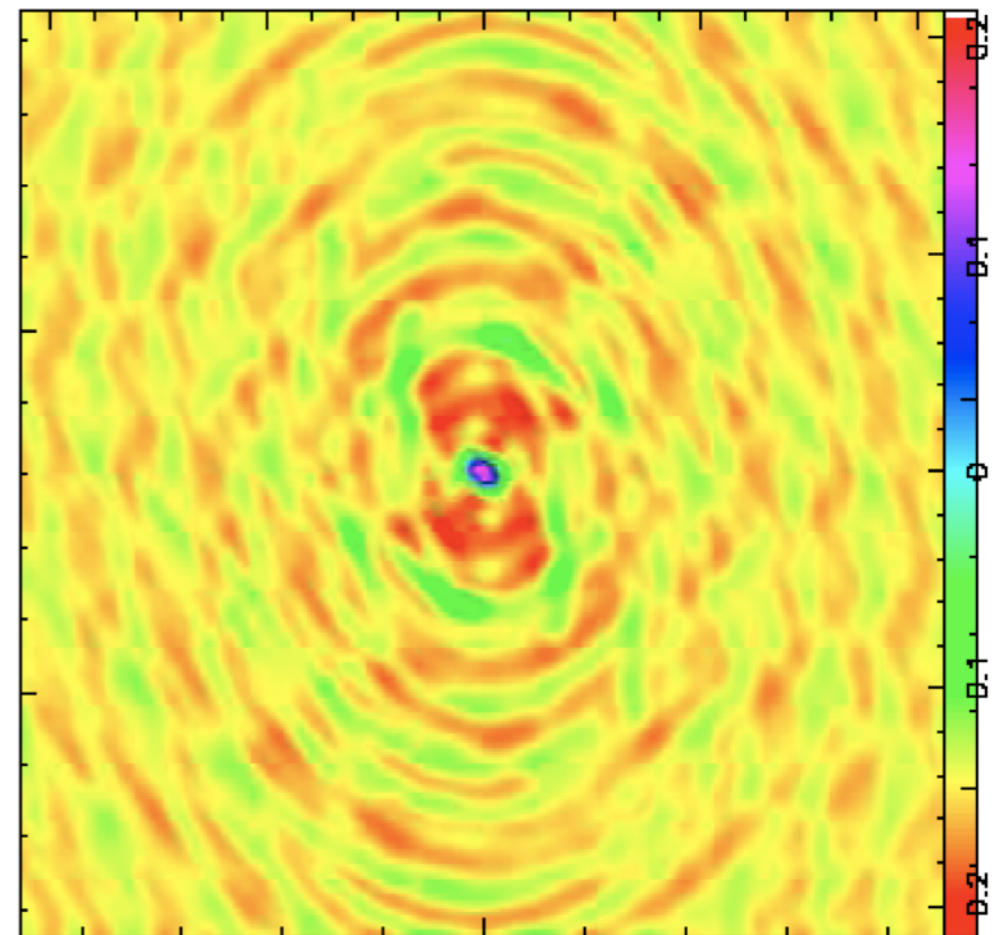


Radar Interferometry

CARMA (USA)



Fourier sampling
(Earth's rotation)



Linear
reconstruction

Structured Measurements

Gaussian matrices: intractable for large N .

Random partial orthogonal matrix: $\{\varphi_\omega\}_\omega$ orthogonal basis.

$$\mathcal{K}f = (\langle \varphi_\omega, f \rangle)_{\omega \in \Omega} \quad \text{where } |\Omega| = P \text{ uniformly random.}$$

Fast measurements: (e.g. Fourier basis)

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Fourier/Diracs: $\mu = 1$. Wavelets/noiselets: $\mu \approx 1$.

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Theorem: with high probability on Ω , $\Phi = \mathcal{K}\Psi$

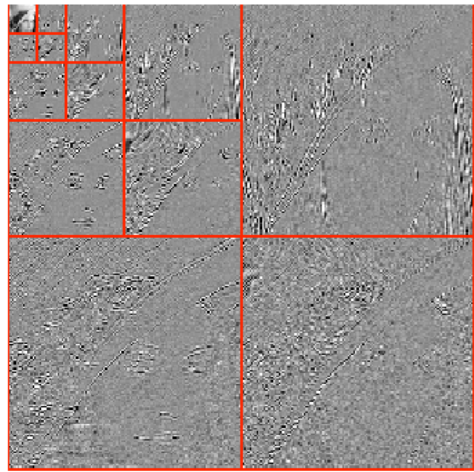
$$\text{If } M \leq \frac{CP}{\mu^2 \log(N)^4}, \text{ then } \delta_{2M} \leq \sqrt{2} - 1$$

[Rudelson, Vershynin, 2006]

→ not universal: requires incoherence.

Conclusion

Sparsity: approximate signals with few atoms.

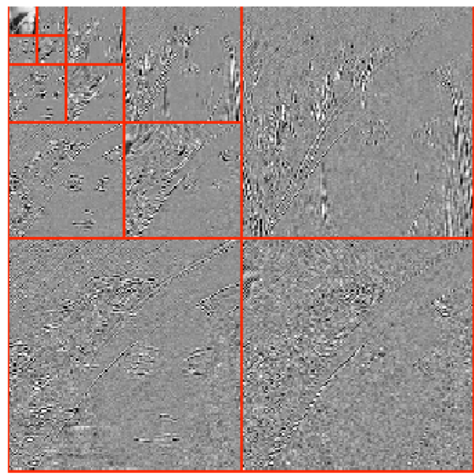


sparsifying
dictionary →

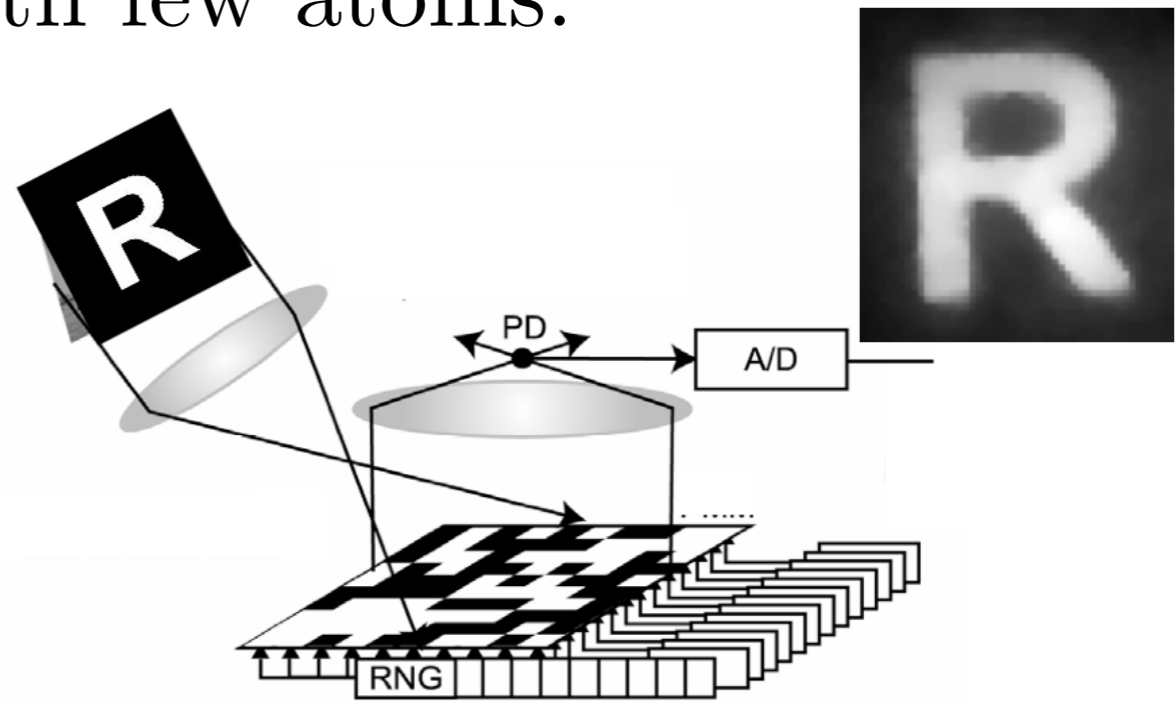


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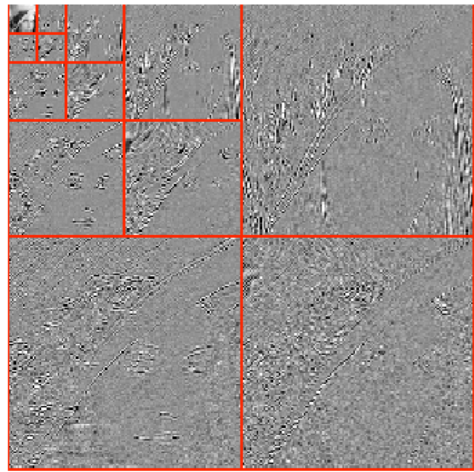


Compressed sensing ideas:

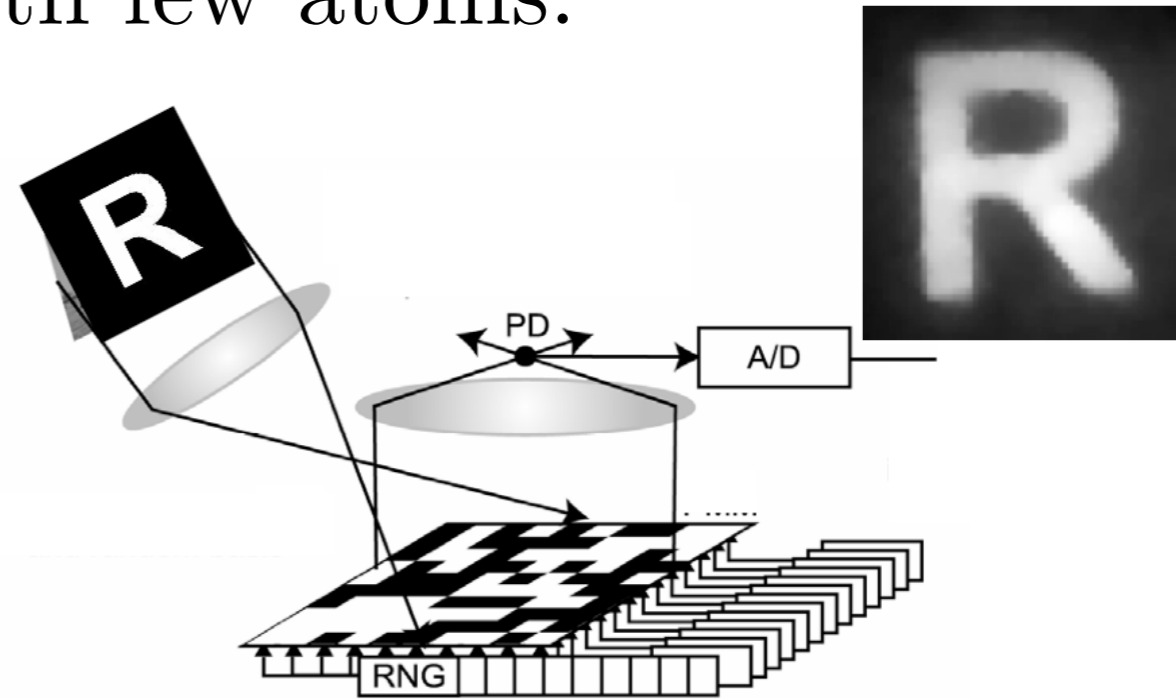
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- Number of measurements \approx signal complexity.
- CS is about designing new hardware.

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sparsifying
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The devil is in the constants:

- Worse case analysis is problematic.
- Designing good signal models.